

# Experimental techniques in nuclear and particle physics

(part 3)

S. Tavernier & D. Kotlinski

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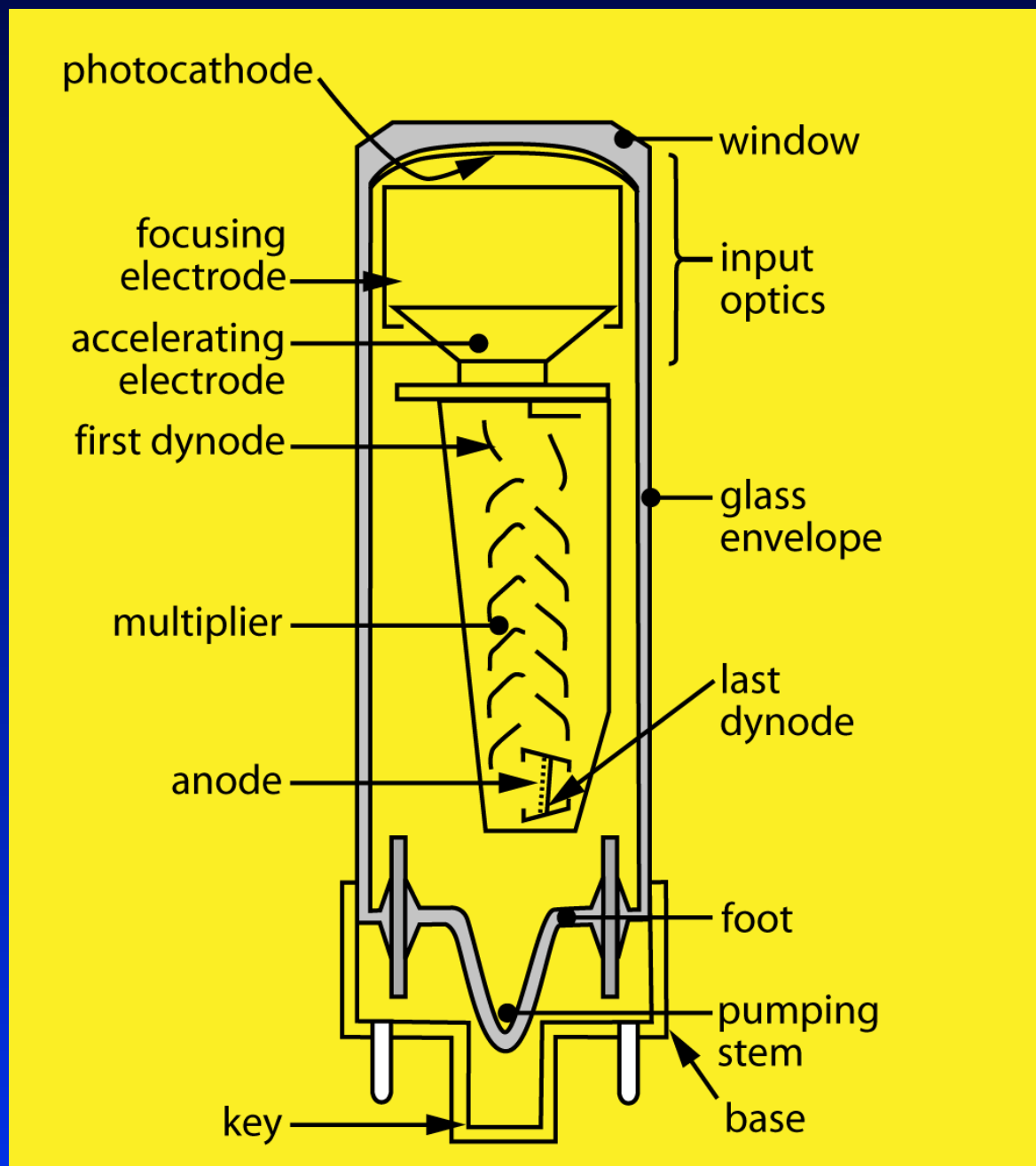
- Interactions of energetic subatomic particles in matter
- Introduction to detectors and detector techniques
- Detectors based on ionisation in gases
- Detectors based on ionisation in semiconductors
- **Detectors based on scintillation**
  - photodetectors
  - physics of scintillation
  - applications of scintillation detectors

# Photodetectors

- Photomultiplier tube (PMT)
- Other vacuum photodetectors
- Solid state photodetectors



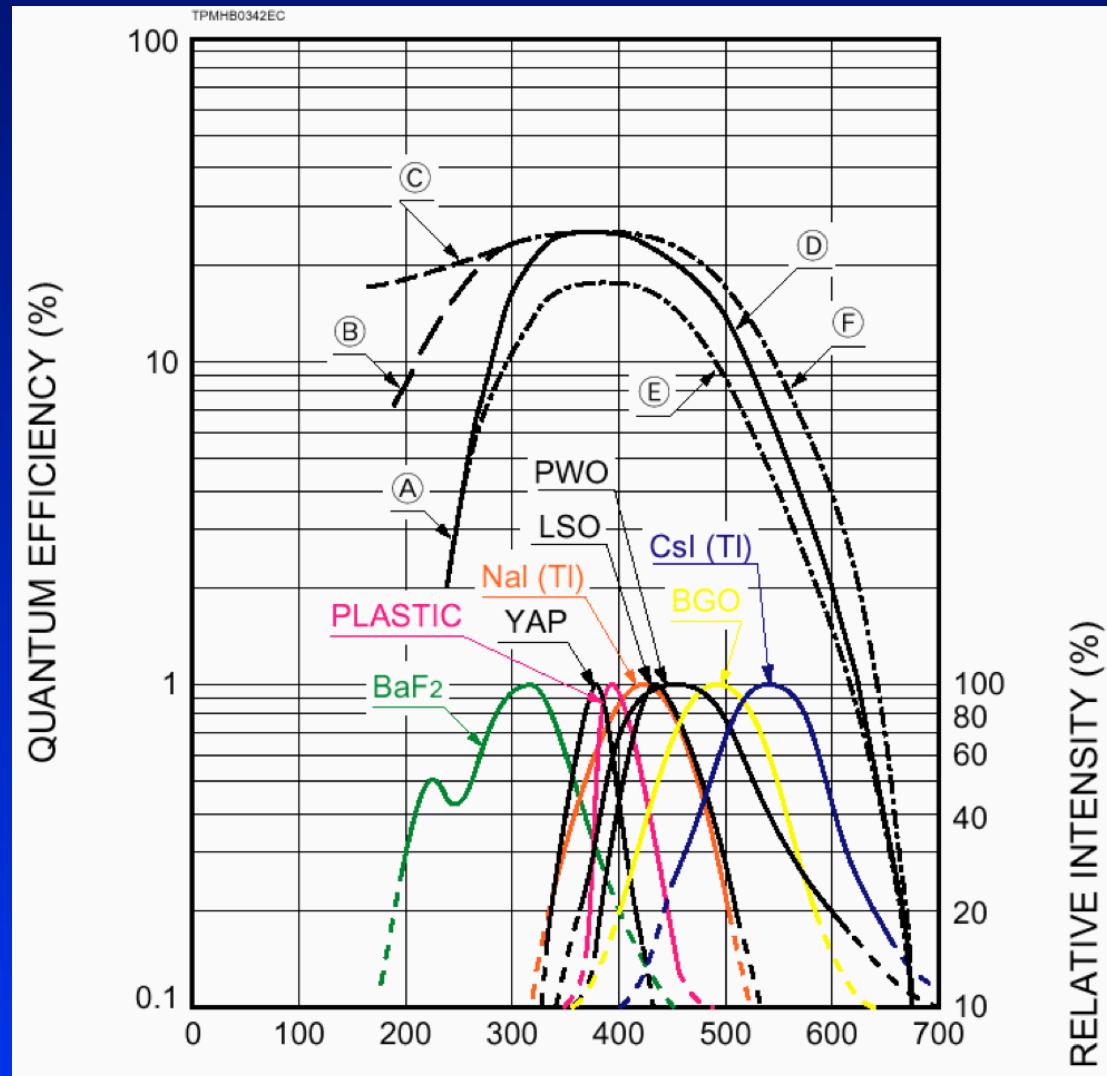
S. Tavernier



IEEE Valencia, Spain, 2011



Quantum efficiency: probability for a photon to give rise to a photoelectron. Electron extracted from the photo-cathode by photo electric effect.



$K_2CsSb$  (Bialkali)  
 $\approx 30\%$

# Dark current

If the photocathode has a large QE

>> easily emission of thermal electrons

>>  $\approx 100$  /cm<sup>2</sup> !!

Source of noise!

# Gain: electron multiplication on dynodes

Typical values:

Total voltage  $\approx 1600\text{V}$ , 12 dynodes

Gain one dynode  $\approx 3$

Total gain  $\approx 10^6$

$$\text{Gain} = a^n \left( \frac{V}{n+1} \right)^{kn}$$

( $a$  ;  $k$ ) constants characteristic of dynode material ( $k \approx 0.7$ )

$n$ : number of dynodes

$V$ : voltage over PM

# Noise considerations

Ideal photodetector & lightsource

$$\frac{\sigma\{S\}}{S} = \sqrt{\frac{1}{N_{\text{photon}}}}$$

Real photodetector

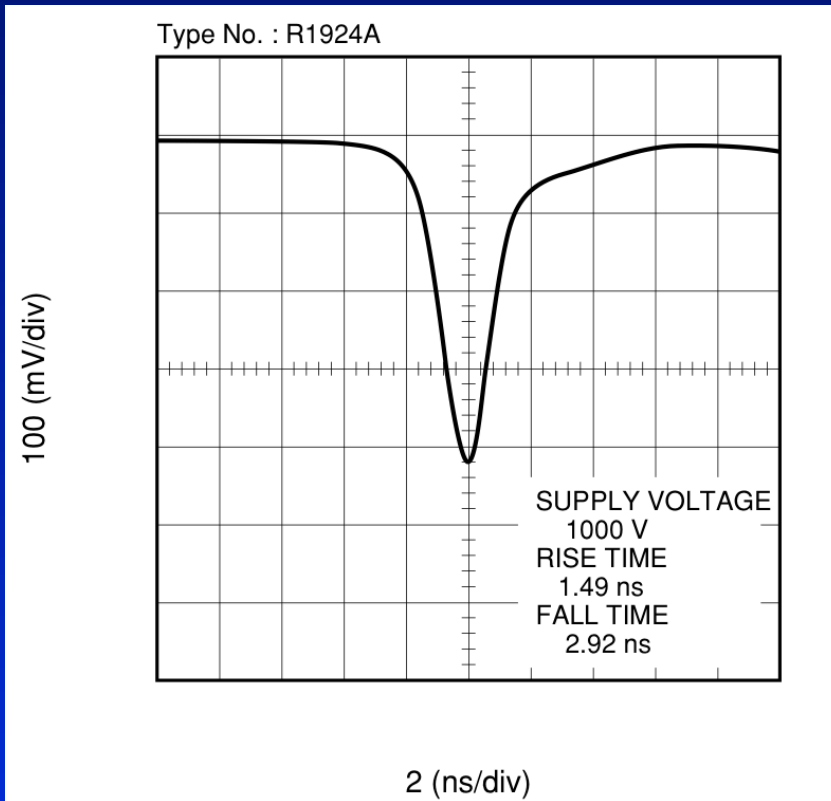
$$\frac{\sigma\{S\}}{S} = \sqrt{\left(\frac{\sigma_{\text{lightsource}}}{S}\right)^2 + \frac{ENF}{QE \times N_{\text{photon}}} + \left(\frac{ENC / e}{Gain \times QE \times N_{\text{photon}}}\right)^2}$$

$$ENC^2 = 2e \times Gain \times \tau \times I_{\text{dark current}} + \frac{32}{3} kTC_d \frac{t_{\text{transit}}}{\tau} + \text{other}(\approx (10e)^2)$$

$$ENF = \left(1 + \frac{\sigma^2\{Gain\}}{\langle Gain \rangle^2}\right)$$

# Timing

## rise time



## time jitter

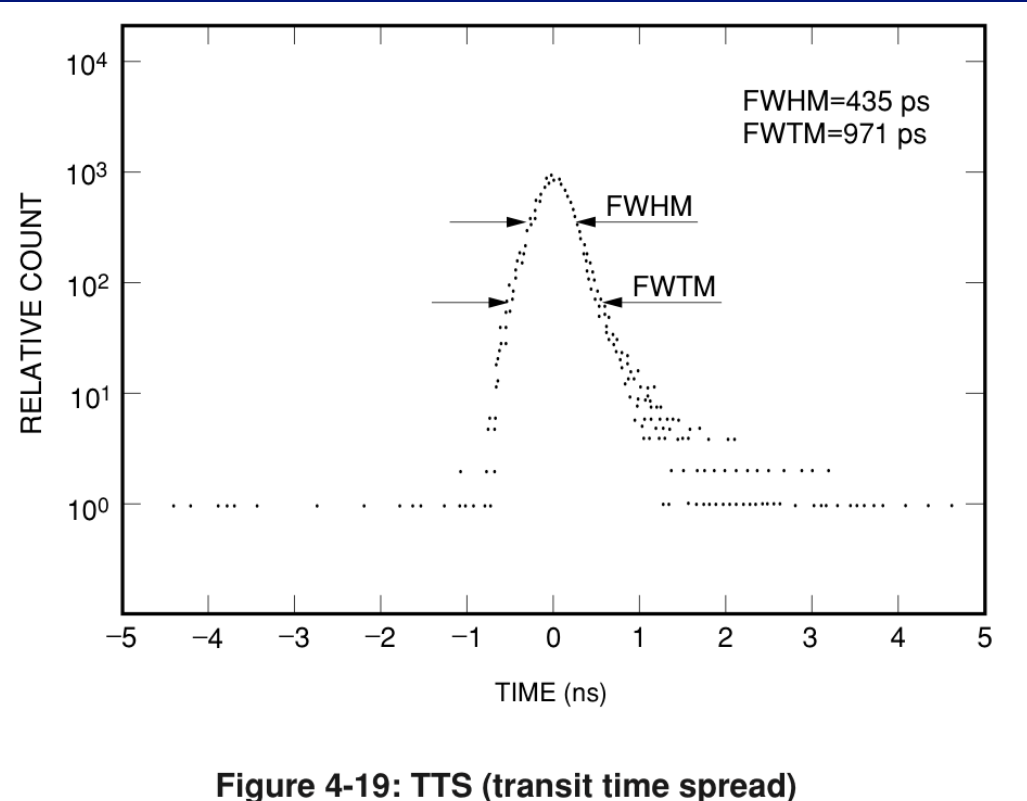


Figure 4-19: TTS (transit time spread)

Good timing need large signal /noise

# Summary on PMTs

- large area: (relatively) inexpensive/unit area
- large gain:  $\approx 10^6$
- Quantum Efficiency  $\approx 30\%$
- excess noise factor:  $\approx 1.3$
- timing:  $\approx 1$  ns
- dark current:  $\approx 100e/s/cm^2 \times \text{gain}$

However:

- bulky
- very sensitive to magnetic fields
- not easily subdivided in pixels

# Other photodetectors

## Other vacuum photodetectors

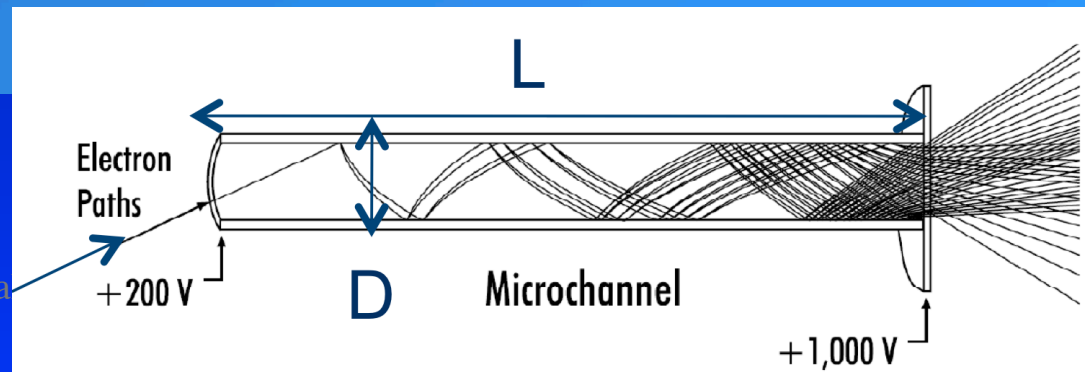
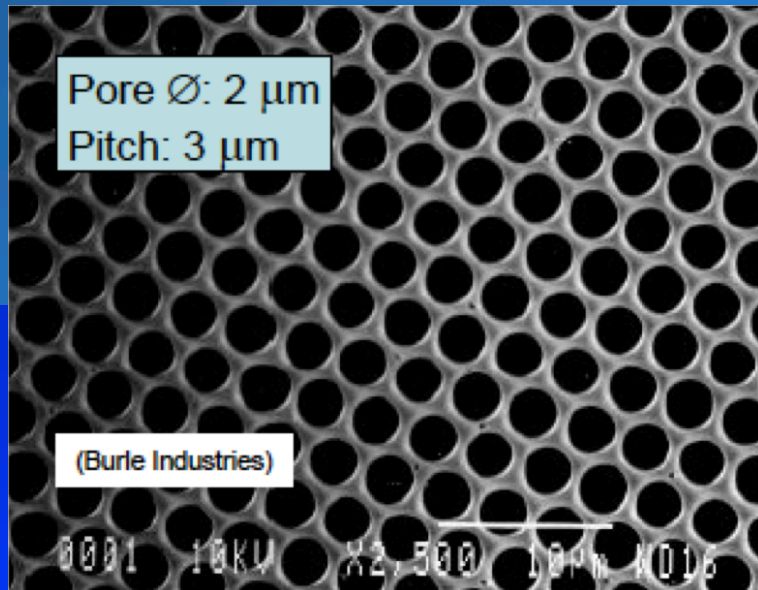
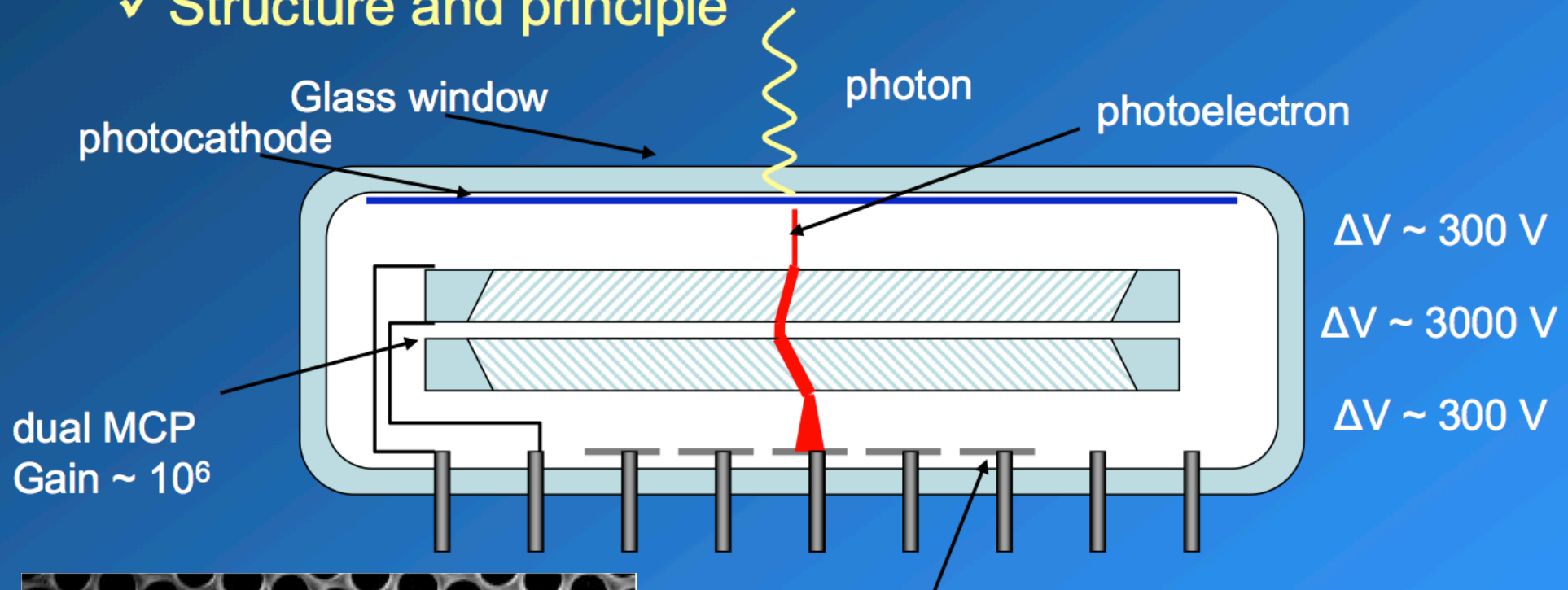
- Microchannel plate PMT
- Hybrid Photon Detector

## Solid state photodetectors

- Photo diodes
- Avalanche photo diodes APD
- Silicon PMT

# Microchannel plate PMT ; MCP-PMT

## ✓ Structure and principle





# Main characteristics of MPC-PMT

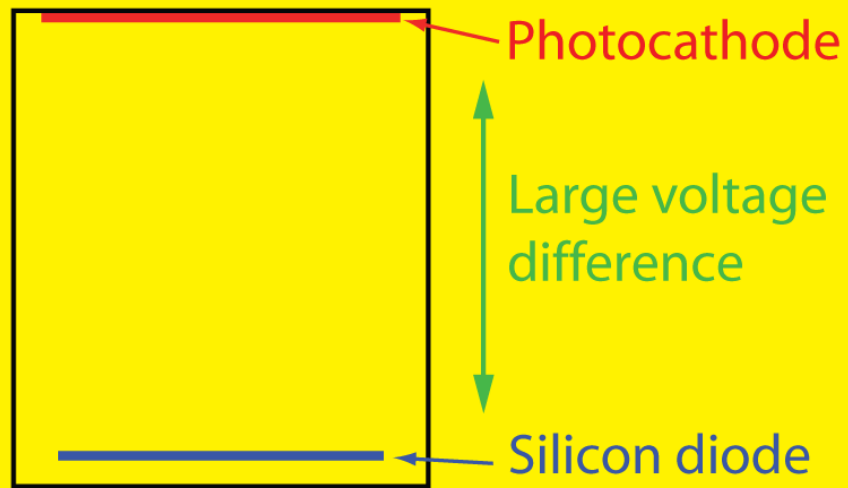
QE:  $\approx 30\%$

Gain: single stage :  $10^3$ – $10^4$  • Dual:  $10^6$ – $10^7$

Good timing properties:

- Low transient time  $\approx 1$  ns
- Transient time spread  $\approx 100$  ps
- Sub-ns rise and fall time

# Hybrid photon detector



(a)



(b)

# Main characteristics of hybrid photon detector

- QE:  $\approx 30\%$
- Excess noise factor  $\approx 1$
- excellent single photon detection efficiency
- Gain=  $\Delta V/3.62 \approx \text{few } 1000$ , but with APD  $\approx 10^5\text{--}10^6$
- easy subdivision in pixels
- bulky and expensive
- very high voltage

# Solid state photodetectors

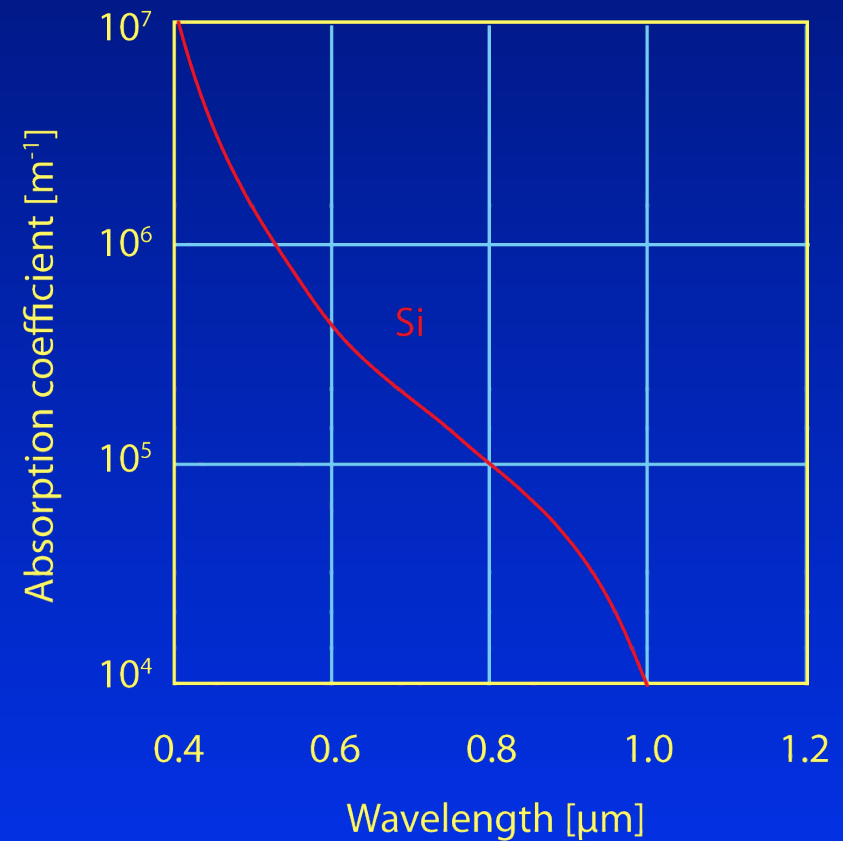
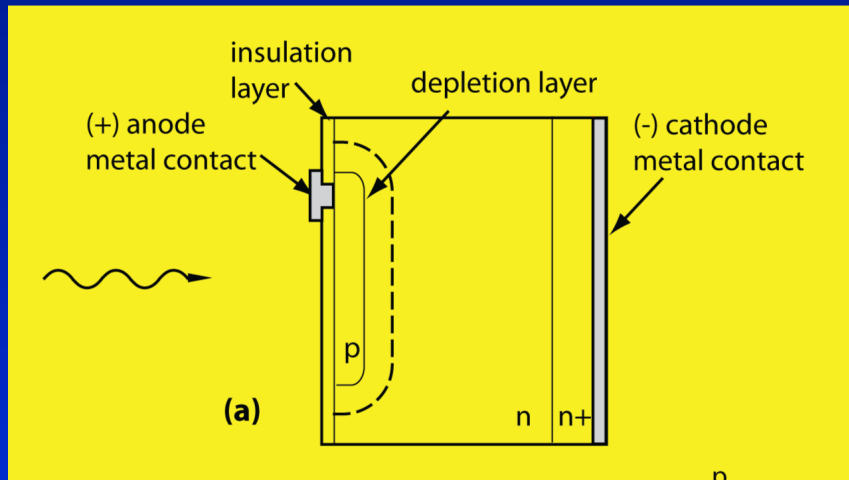
Photo diode

Avalanche Photo Diode

SiPM

# Silicon photodiodes

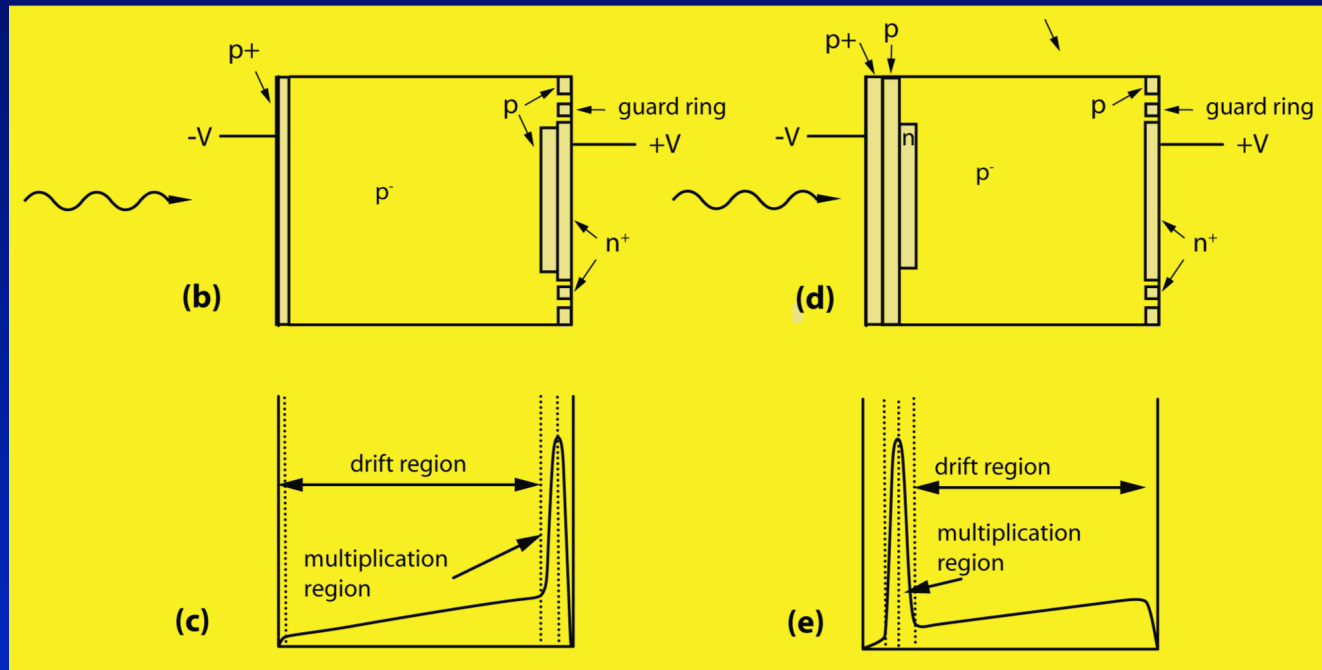
Electron from valence band to conduction band



# Main characteristics of silicon photodiodes

- No internal gain
- large QE  $\approx 80\%$
- insensitive to magnetic fields
- low dark current

# Avalanche photo diodes

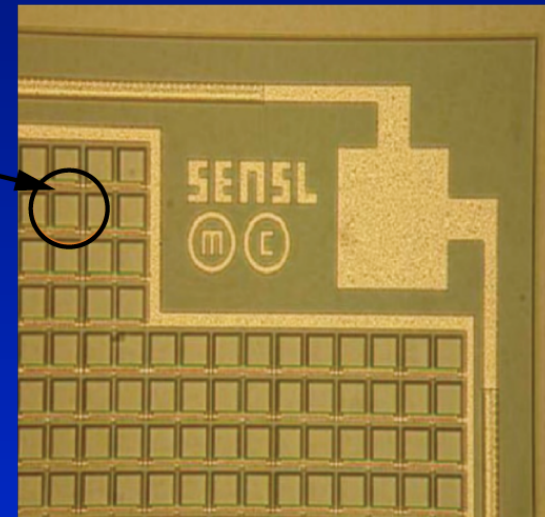
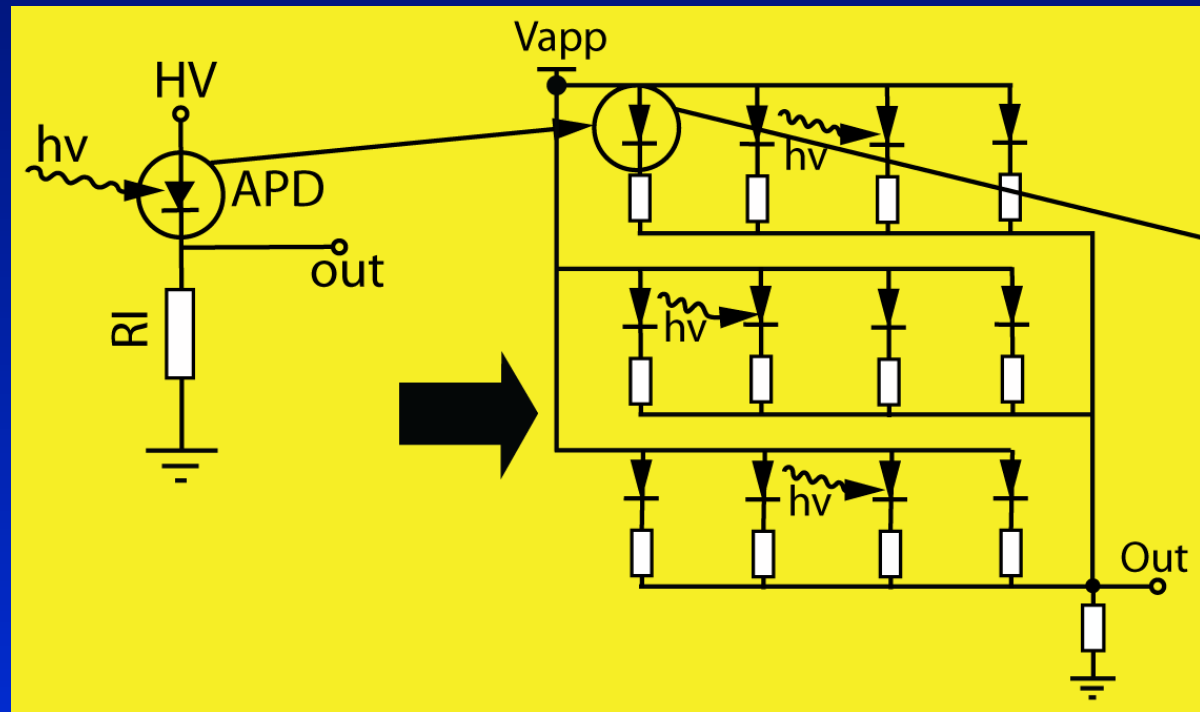


# Main properties Avalanche photo diodes

- moderate gain  $\approx 50$
- QE  $\approx 70\%$  @ 400 nm;  $80\%$  @ 500 nm
- insensitive to magnetic field
- dark current  $< \approx 1$  nA/mm<sup>2</sup>
- excess noise factor  $\approx 2$
- gain very dependent on temperature and applied voltage



# SiPMT, Geiger mode APD, MPPC



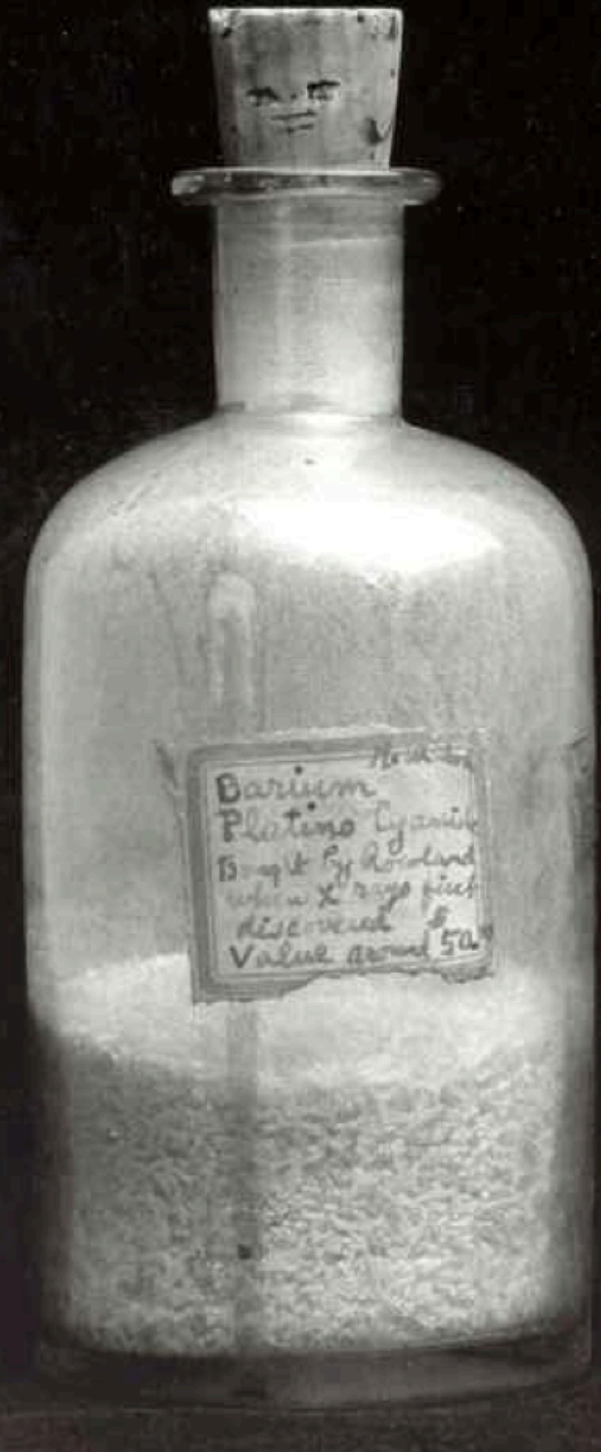
# Main properties of SiPM

- Large gain  $\approx 10^6$
- insensitive to magnetic fields
- photon detection efficiency =  $QE \times \text{Fill\_factor}$   
10%-50%
- excess noise factor  $\approx 1$
- large dark current  $\approx 10^6$  pulses/mm<sup>2</sup>  $\approx \mu\text{A/mm}^2$

# The physics of scintillation

# Introduction to scintillators

Scintillators also are among the oldest particle detectors. Röntgen discovered X-rays by observing a faint light emission from barium platino-cyanide. This was really the first observation of scintillation. Scintillation was also used by Rutherford in his famous scattering experiments. Rutherford used zinc sulfide to detect alpha particles.



Many transparent materials give off a faint light pulse when an energetic subatomic particle deposits energy. This is called radio-luminescence.

If large pieces >> called scintillators

If powder >> called phosphors, but the word phosphors is also use for photo-luninescent materials (=wavelength shifters or fluors)

If a charged particle causes ionisation in a solid, the charges will (in general) not be extracted if a voltage is applied over the solid.

But to cause scintillation the charges only need to get to the nearest luminescence centre, and that is possible in many materials.

Scintillators broadly fall into two classes with very different properties and applications

- Organic scintillators:
  - mainly used for charged particle tracking
  
- Inorganic scintillators: mainly used for
  - gamma spectroscopy
  - as phosphors for X-ray imaging (radiology)

# Organic scintillators

**Crystalline solids:** anthracene, stilbene: today hardly ever used

**Organic liquids:** Liquid containing aromatic rings: e.g. (1,2,4-trimethylbenzene) and linear alcaylbenzene (LAB); + wls fluors dissolved in it: e. g. p-Terphenil, PPO (2,5-Diphenyloxazole)

**Plastics scintillators:**

A plastic organic scintillator is a polymerizable organic compound (methylmethacrylate, vinyltoluene, styrene) containing aromatic rings, + wls fluors dissolved in it at 1% level

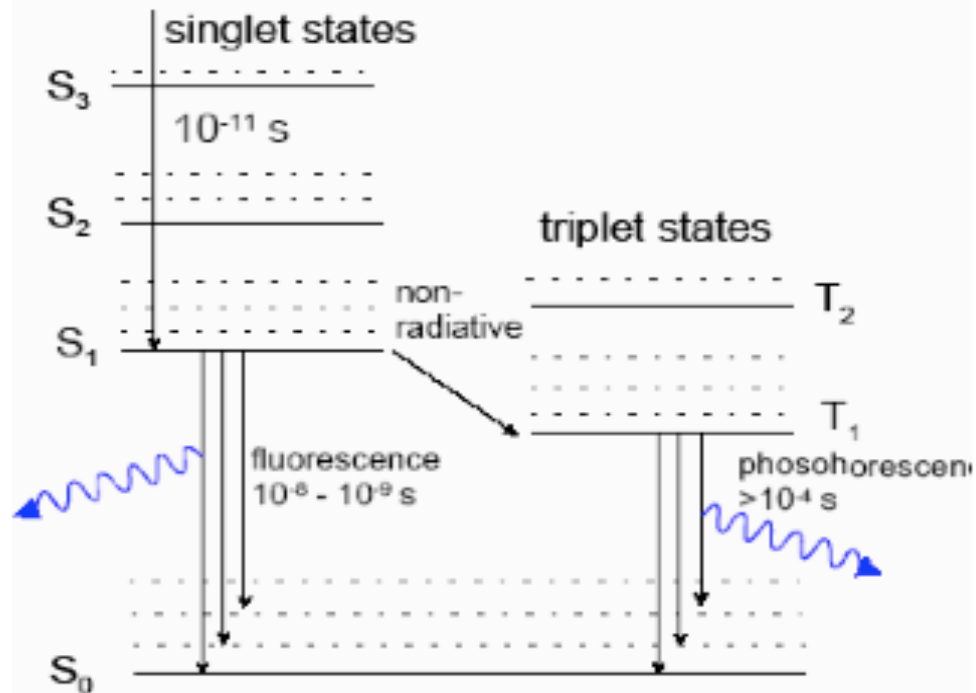
# Liquid and plastic scintillators

organic scintillators low Z (C,H) →

- low  $\gamma$ -detection efficiency
- high n-detection efficiency via (np)

scintillation mechanism:

## Delocalized p electron states of the Benzene molecule



The liquid or plastic base scintillates in the UV, but the m.f.p of this emission is very short ( $\ll 1\text{mm}$ ). One or more "fluors" (i. e. wale length shifters) are dissolved in the plastic. The primary fluor ( 1%) shifts this to longer wavelength, often a secondary fluor (0.05%) is added to shift the emission to even longer wavelengths.



# Properties of plastic scintillators.

(Just one typical example)

Kowaglass SCSN-32, polystyrene based scintillator

Light yield: 8'000 photons /MeV, or  $\approx 16'000$  photons/cm

Decay time : 3.6 ns

Emission wavelength: 423 nm

Light attenuation length: 250 cm

Refractive index : 1.58

Density : 1.08

Radiation length : 30 cm

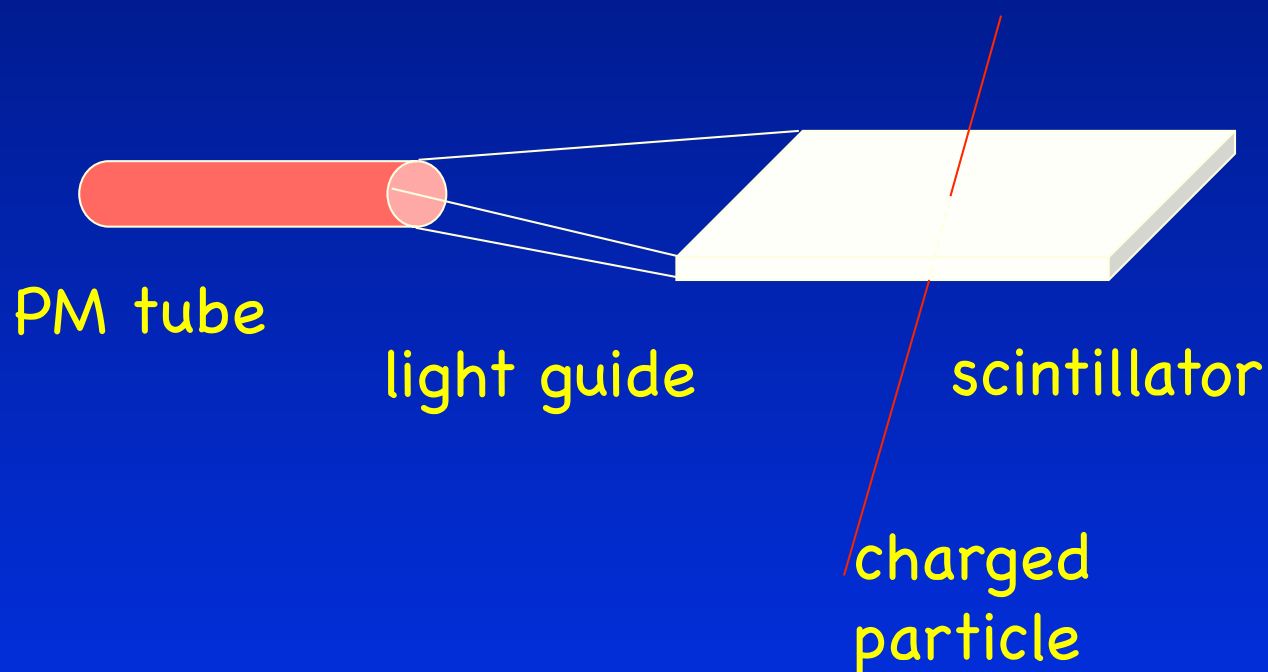
The biggest advantage of plastic scintillators is the ease of mechanical processing, availability in large sizes, often as sheets, and also as scintillating fibres

Liquid Scintillators have a very reduced light response to heavily ionising particles such as alpha particles or nucleons with an energy in the MeV range.  
Light yield depends on ionisation density (Birks' law).

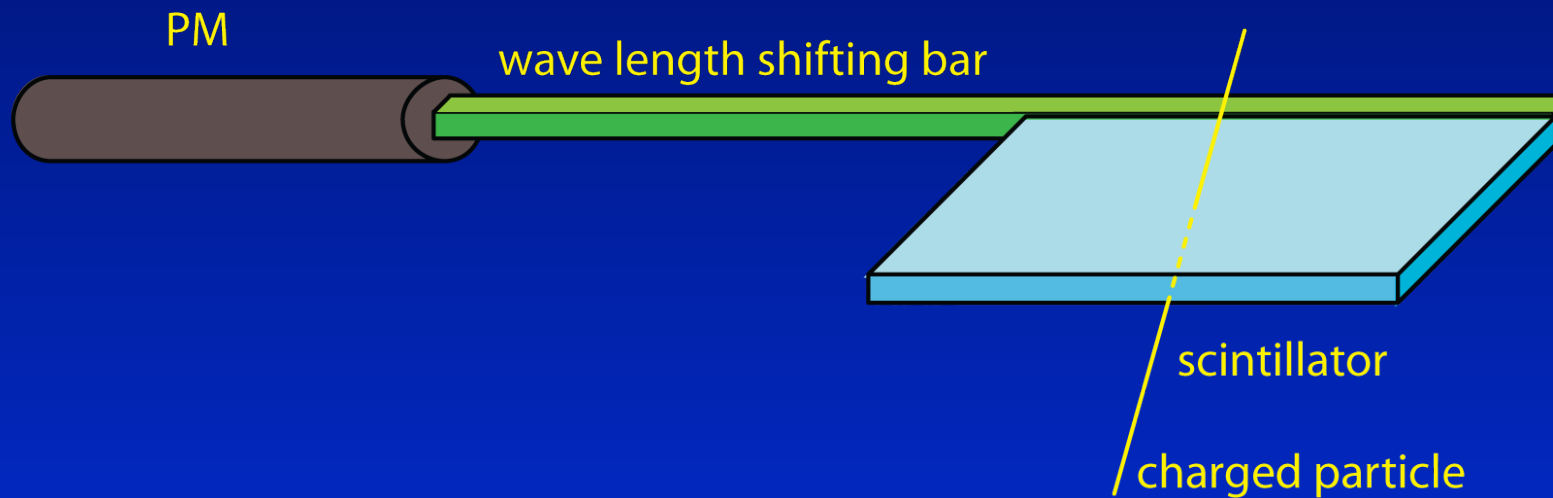
$$\frac{d(LY)}{dx} = (LY)_0 \frac{dE / dx}{1 + k_b(dE / dx)}$$

A plastic scintillator used as a detector of charged particles, light guided to the edge by internal reflection.

When using a light funnel, the surface of the photodetector should be equal the surface of the edge



Wave length shifter readout is more efficient if a large surface needs to be read





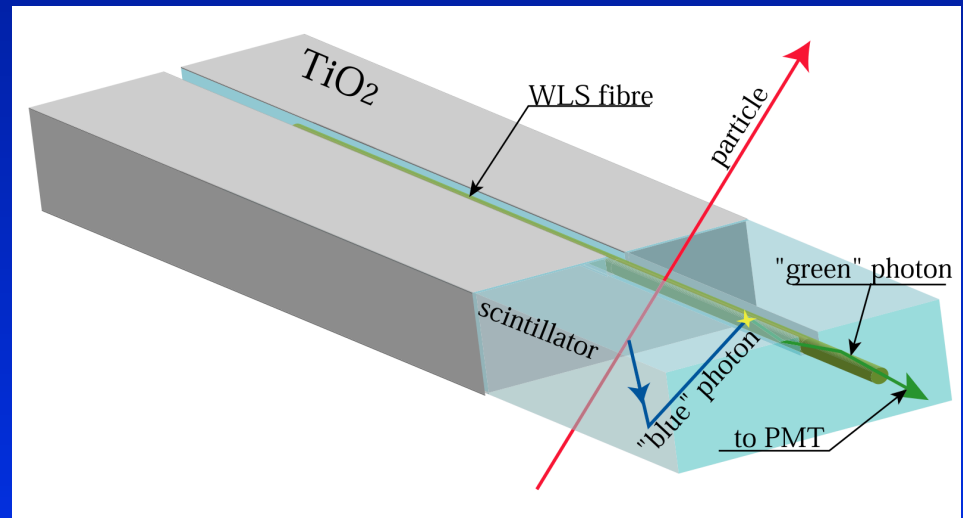
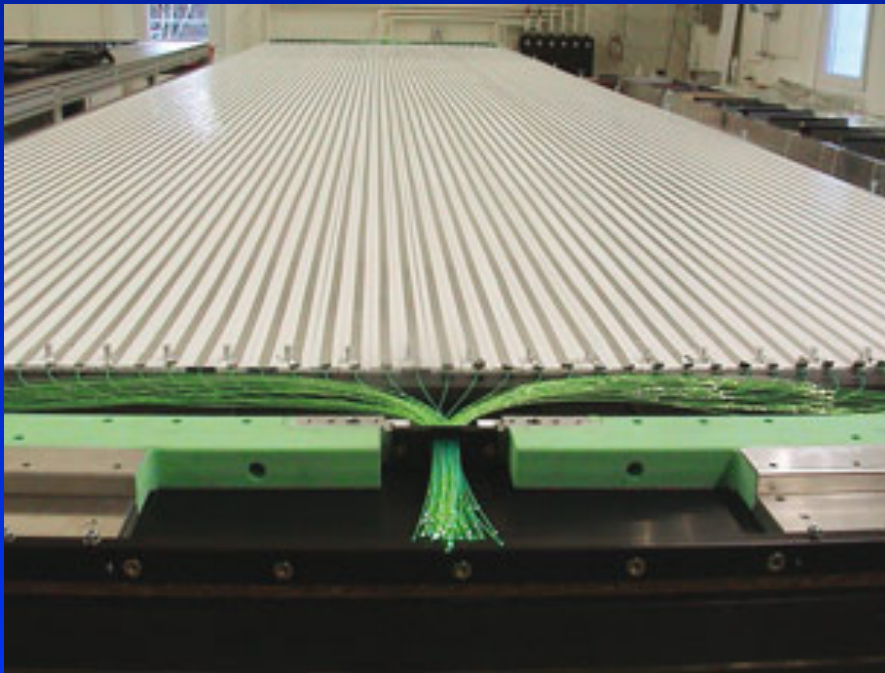




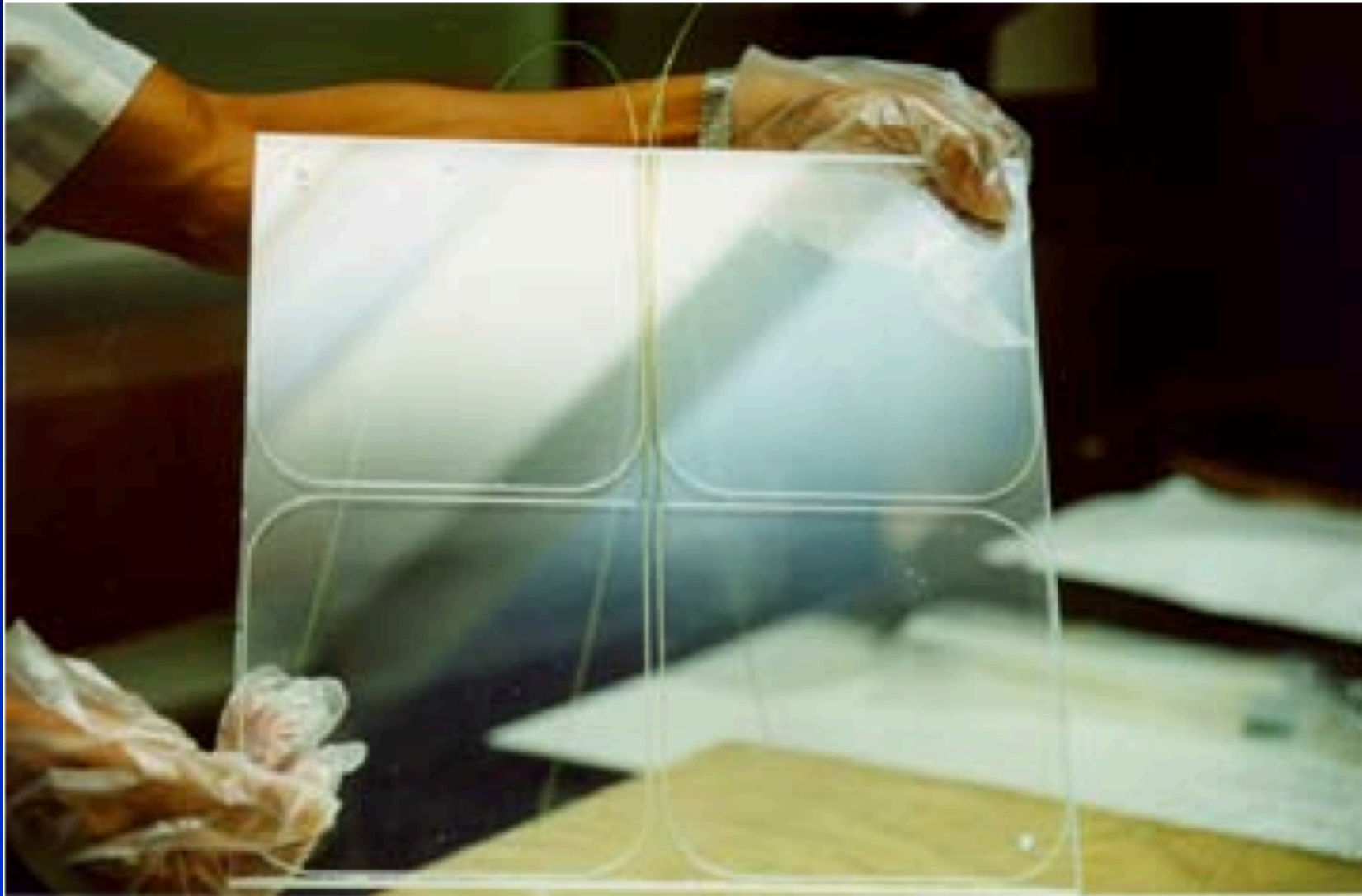
## Applications of liquid & plastic scintillators

Plastic: particle tracking and timing

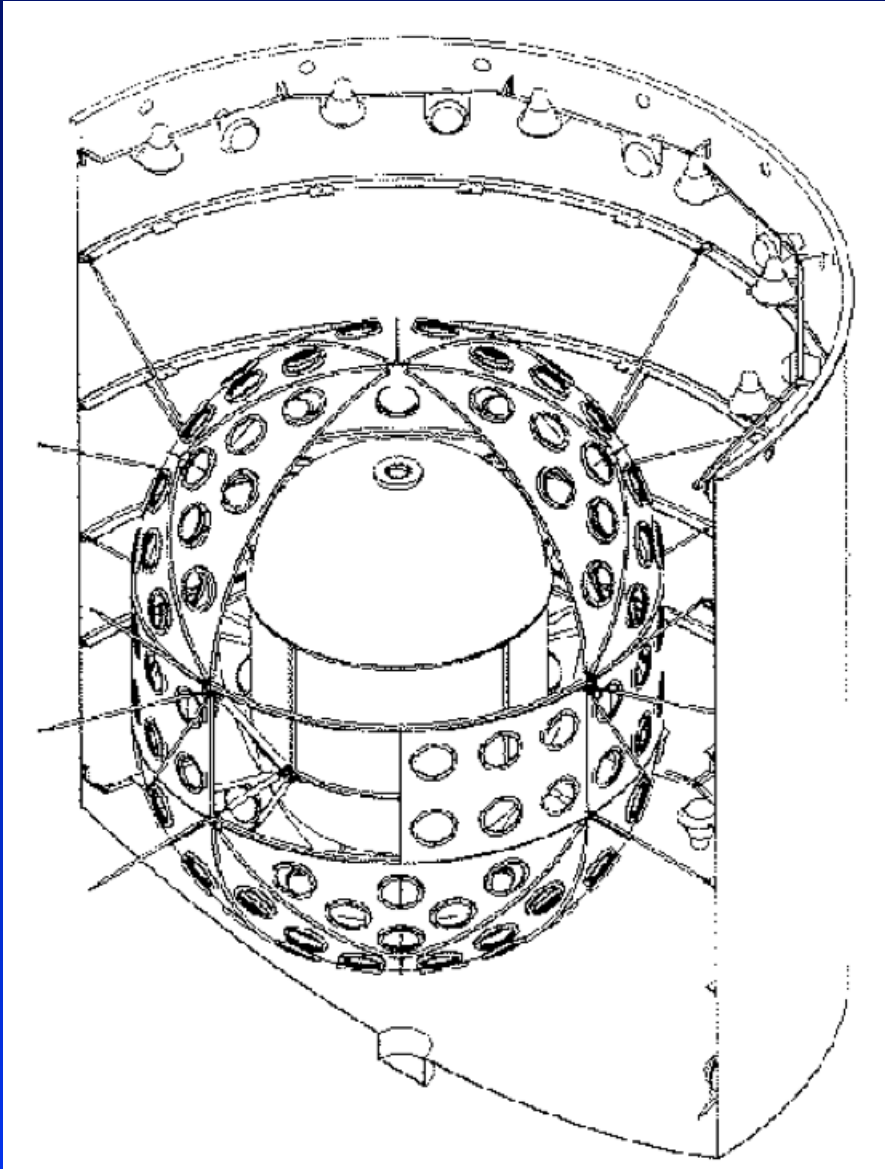
Example: OPERA neutrino velocity measurement based on signal in plastic scintillator strips with wavelength shifting fibres read on both ends with Hamamatsu 64 channel PMTs.



## WLS fibre readout in CMS hadronic calorimeter



Chooz experiment: liquid scintillator  $\approx 110$  tons liquid scintillator  
Nuclear reactor  $\approx 10^{21}$  anti neutrino/s  $\approx 1.5$  MeV

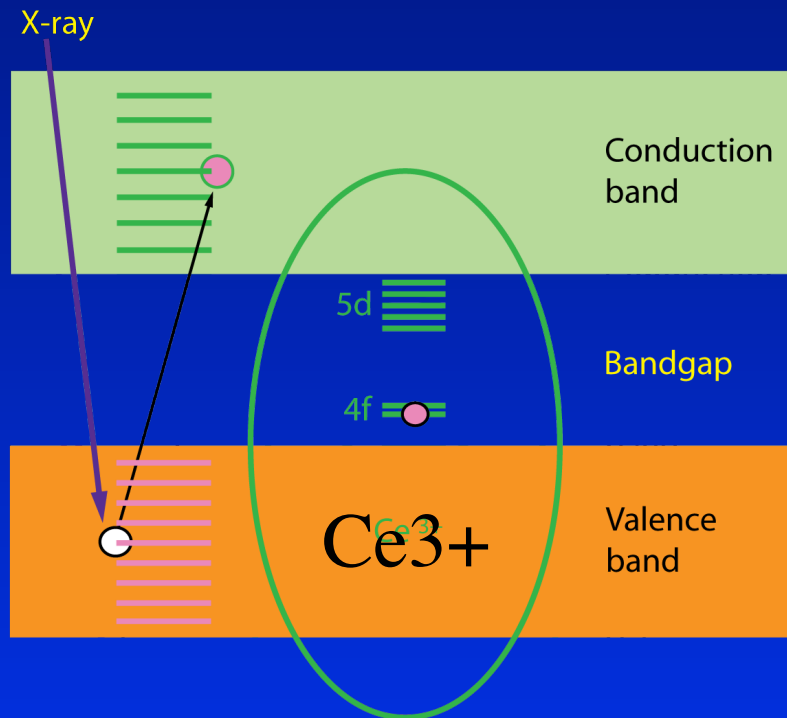


- (1) Gd loaded scintillator to detect neutron ( $\approx 8$  MeV)
- (2) unloaded scintillator: positron energy and 2x gamma from  $e^+$  annihilation ( $\approx 3$  MeV)
- (3) veto shield scintillator



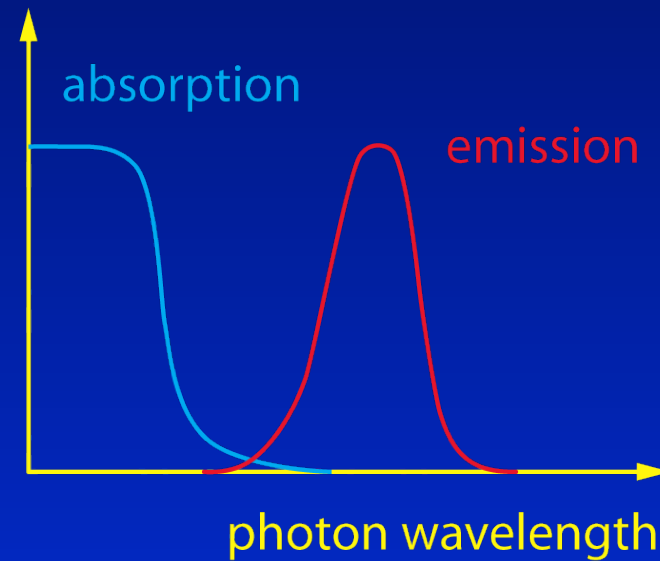
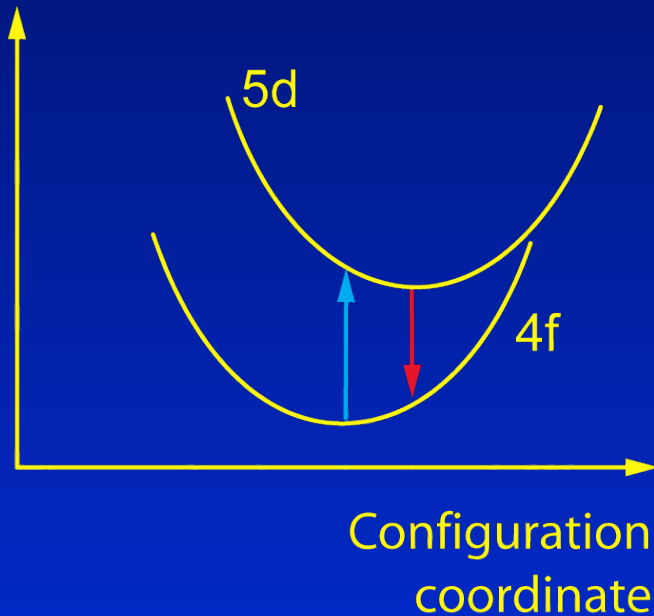
# Inorganic scintillators

Usually ionic crystals with luminescence centres, e.g.  $\text{Ce}^{3+}$  at the % level.



# The Stokes shift allows the light to leave the crystal

Electron energy



# How is scintillation generated in inorganic solids?

STEP 1: gamma-ray interaction gives rise to a large number of e-h pairs **after**  $\approx 10^{-12}$  s. (free or excitons)

$$N_{e-h} = \frac{E_{\gamma}}{b \cdot E_{BG}} \quad [E_{BG} = \text{energy bandgap}]$$

$E_{\gamma}$  = energy gamma ray

$b = 1.5 - 2$  for ionic crystals

Maximum yield: 
$$N_{e-h} \approx \frac{1}{2} \cdot \frac{1'000'000}{E_{BG}[eV]}$$

CsI:Tl  $E_{BG} = 6.2 \text{ eV}$

$\Rightarrow N_{\max} = 80'000 \text{ Photons/MeV}$

Experimentally  $65'000 \text{ Photons/MeV}$

## STEP 2:

Electrons and holes reach the luminescence centre, influenced by traps. Most unpredictable part of the process.

## STEP 3:

Excitation and decay of luminescence centre

Most efficient scintillators have extrinsic luminescence centres, also called activators:

NaI:Tl<sup>+</sup>, CsI:Tl<sup>+</sup>, CaF<sub>2</sub>:Eu<sup>2+</sup>, BaFBr:Eu<sup>2+</sup>, Lu<sub>2</sub>SiO<sub>5</sub>:Ce<sup>3+</sup>

But luminescence in absence of an activator also occurs.  
Pure Bi<sub>4</sub>Ge<sub>3</sub>O<sub>12</sub> [BGO] scintillates at 480nm.

BGO is an efficient scintillator at low temperature,  
thermally quenched at room temperature.

## Non-linear response and energy resolution

Scintillators have a very reduced response to strongly ionising particles such as alpha particles or nucleons with an energy in the MeV range.

An alpha particle of 1 MeV will typically produce 0.25–0.8 times less light than a gamma (electron) of the same energy. ( $\alpha/\beta$  ratio)

In alkali halides there is also a reduction in light if the ionisation density is very low

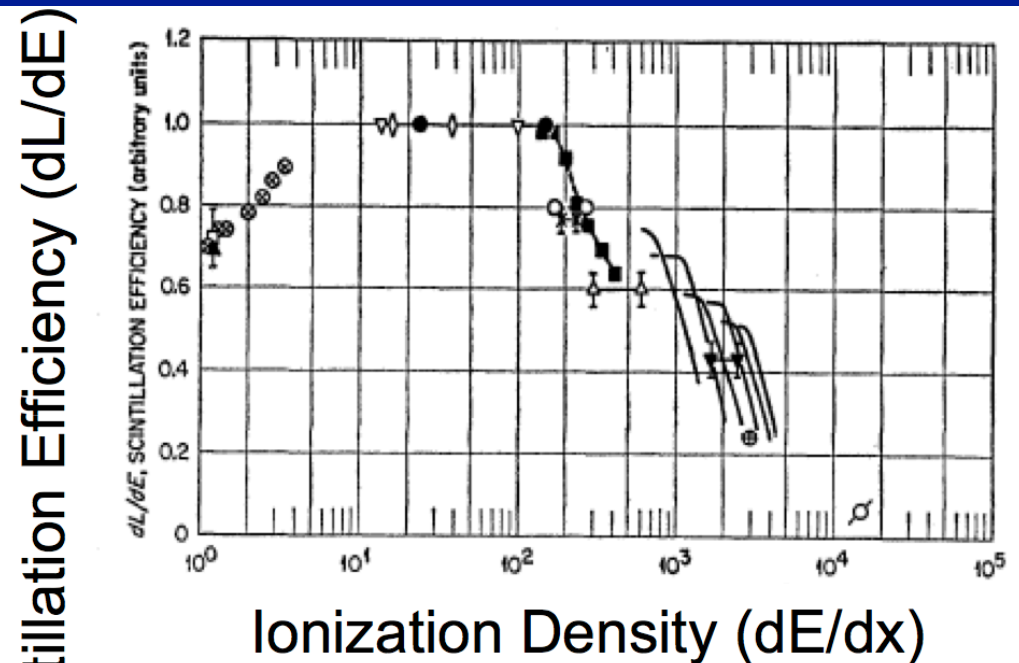
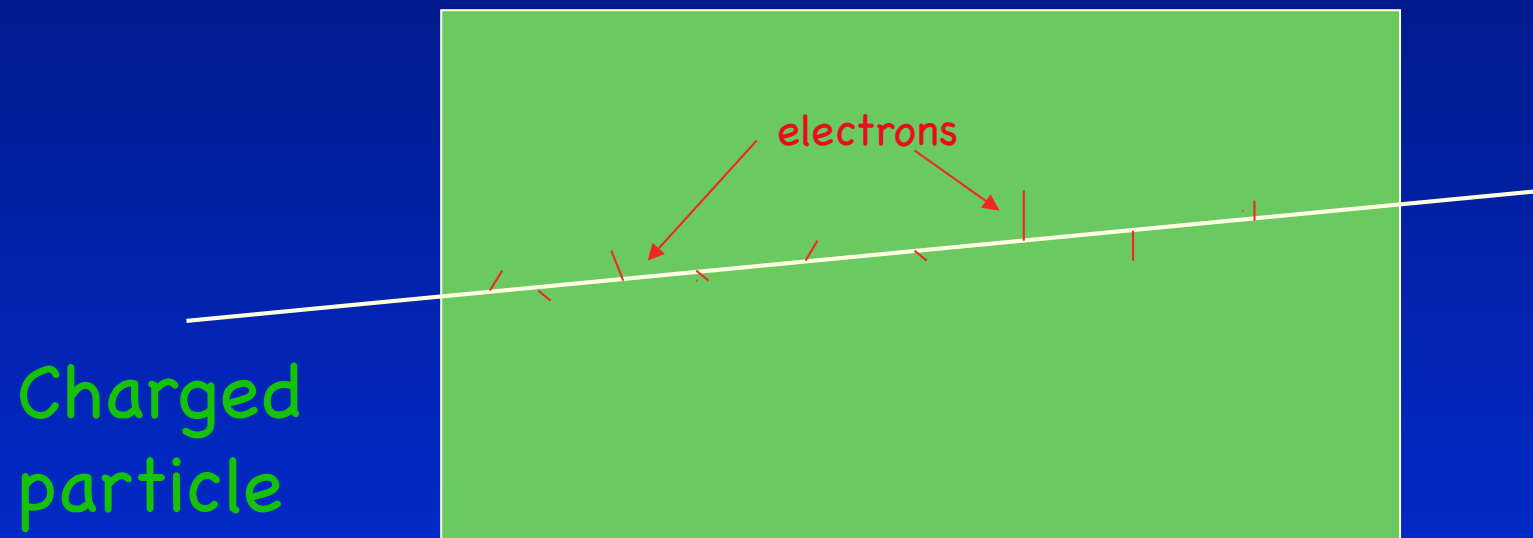
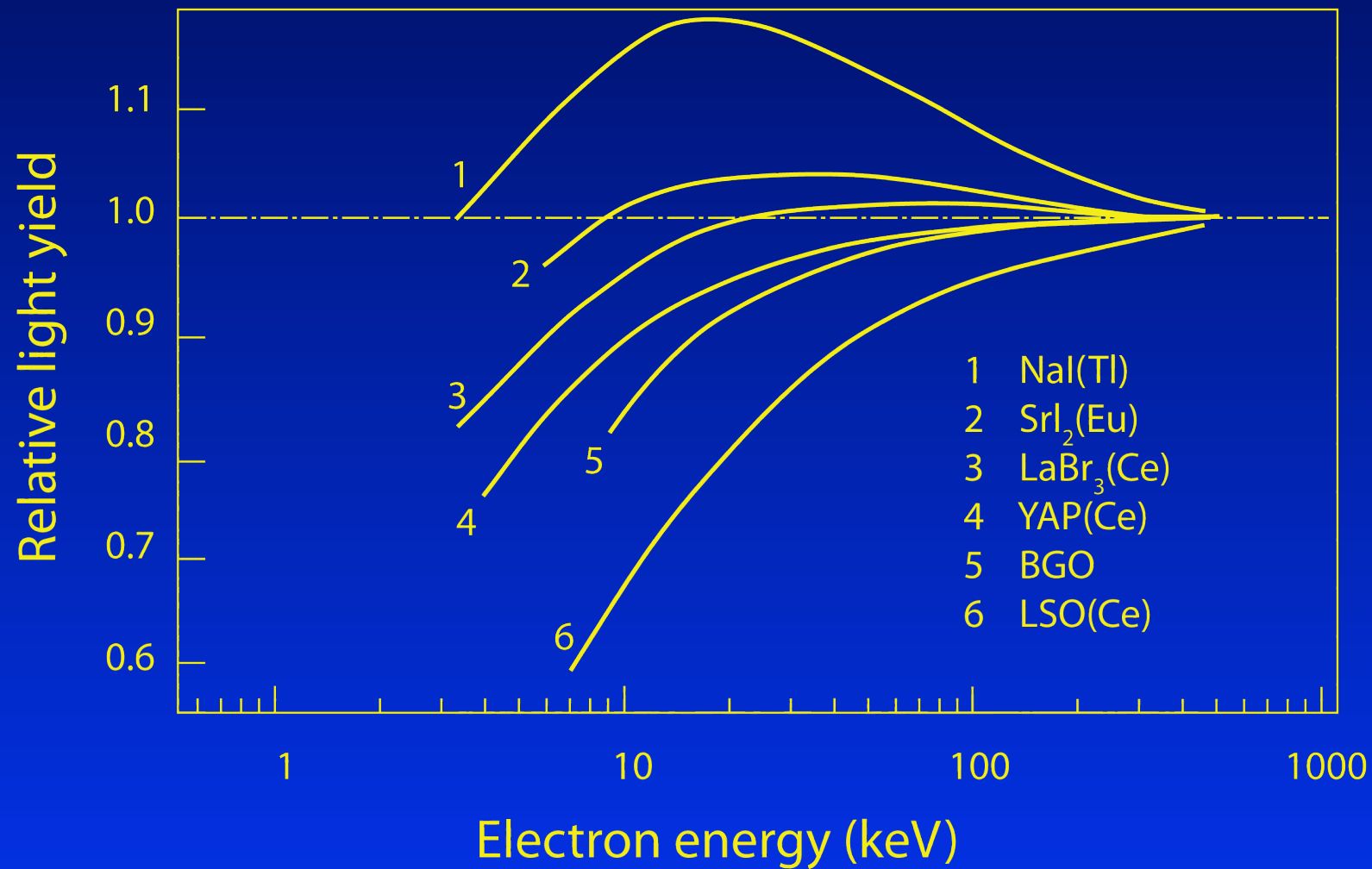


FIG. 2. Scintillation efficiency as a function of  $dE/dx$  for various particles in NaI(Tl).

A single electron track will give rise to a large number of lower energy electron tracks each different ionisation density.



The scintillation signal from an electron is not linearly related to the energy





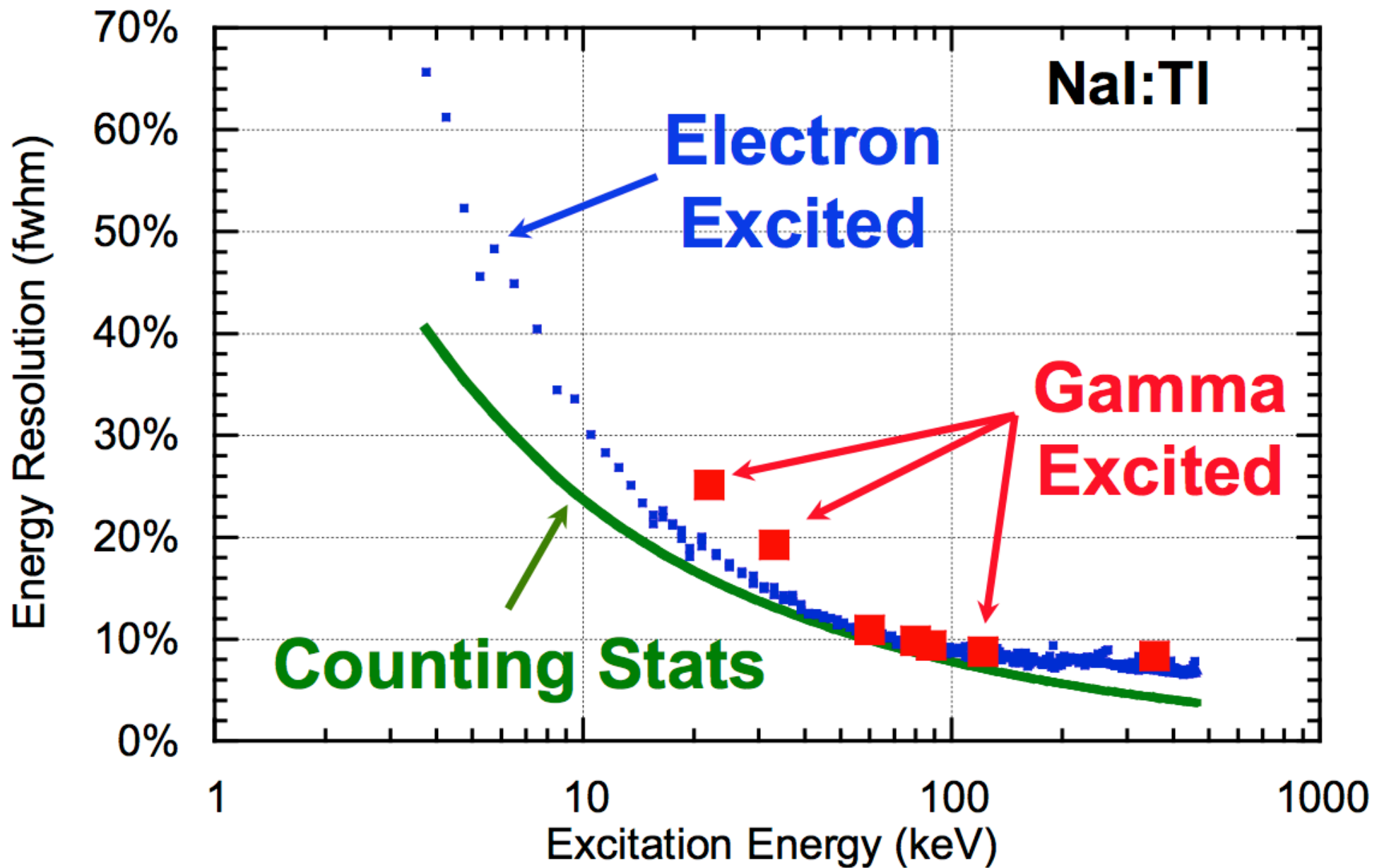
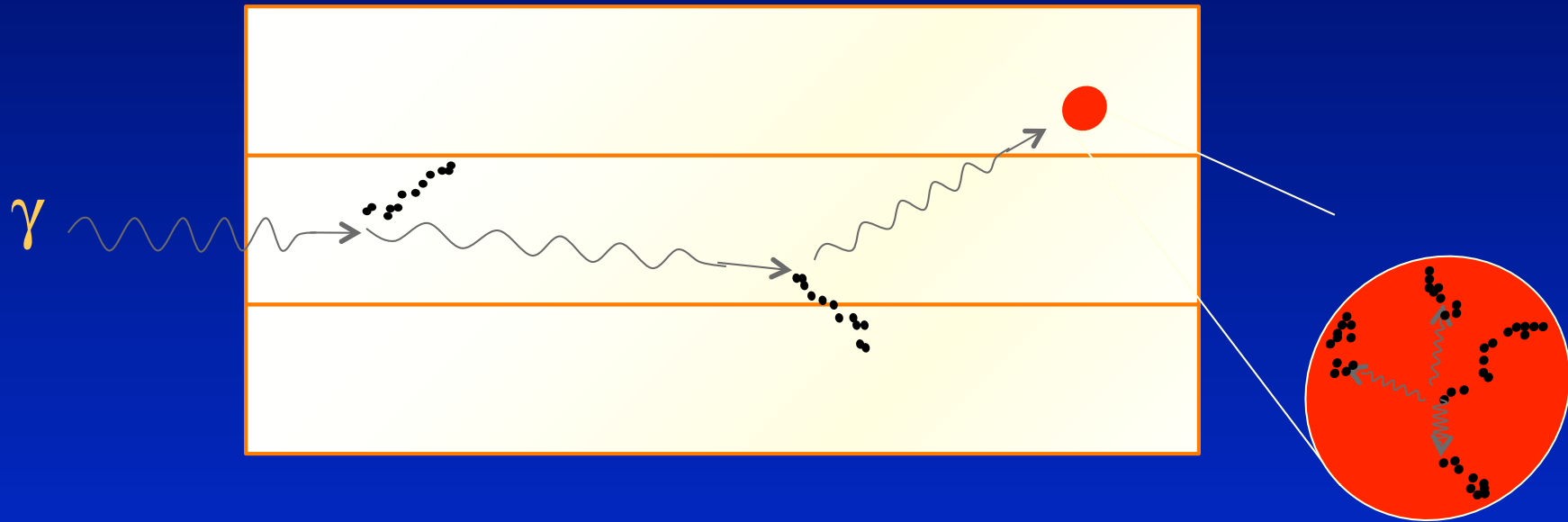


Figure from W.W. Moses, et al., IEEE Trans. Nucl. Sci. NS-55, pp. 1049, 2008

This non linear energy response to electrons results in a degraded energy resolution



In scintillators the light yield depends on the ionisation density. Such an effect is not observed with semiconductors. However, carrier mobility and diffusion in commonly used semiconductors (covalent crystals) are up to 3 orders of magnitude larger than in scintillators (ionic crystals).

## Energy resolution for gamma detection in inorganic scintillator

$$R^2 = R_{\text{intrinsic}}^2 + R_{\text{lightyield}}^2$$

$$R_{\text{lightyield}}^2 \propto \frac{1}{N_{\text{photoelectrons}}}$$

### Intrinsic energy resolutions for a few crystals

NaI:Tl	5.7±0.2 %	
BGO	4.2±0.6 %	
CsI:Tl	5.9±0.3 %	
LSO:Ce	6.6±0.4 %	D=0.02 cm <sup>2</sup> /s
YAP:Ce	1.0±1.0 %	D= 0.1 cm <sup>2</sup> /s

In detector grade germanium; D≈ 200 cm<sup>2</sup>/s

## Decay characteristics

Emission characteristics are determined by the luminescence centre and only moderately influenced by the host matrix

Example  $Ce^{3+}$  decay:  $5d \rightarrow 4f$  allowed dipole transition

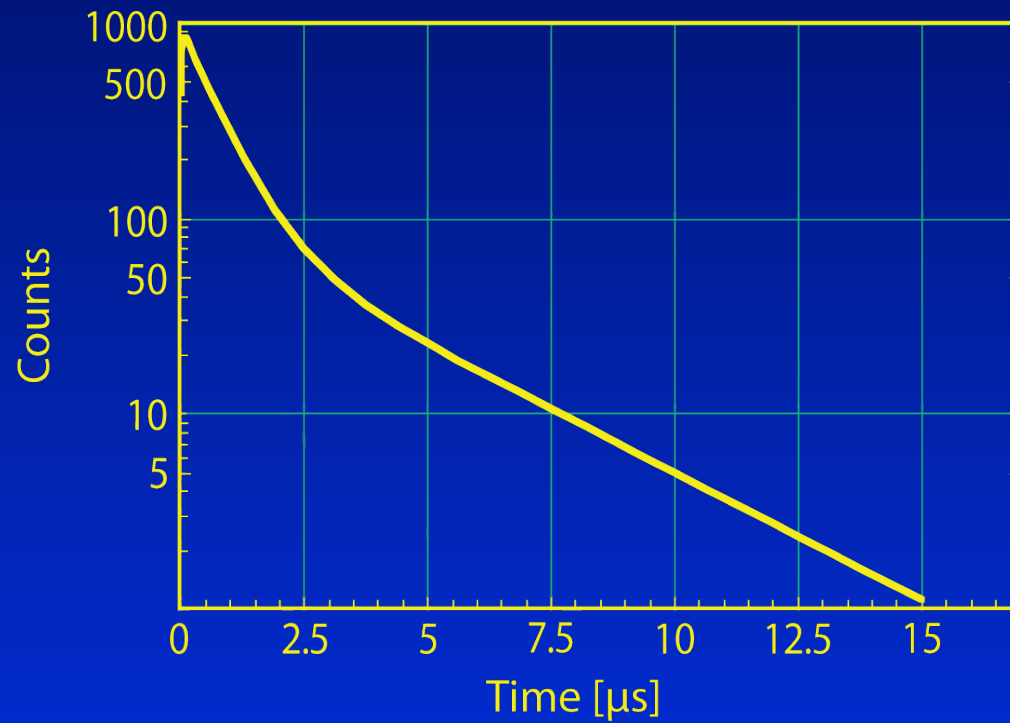
$$\Gamma = \frac{1}{\tau} = \frac{4}{3} (2\pi)^3 \alpha \frac{\nu^3}{c^2} n \left( \frac{n^2 + 2}{3} \right)^2 |\langle i | \vec{r} | f \rangle|^2$$

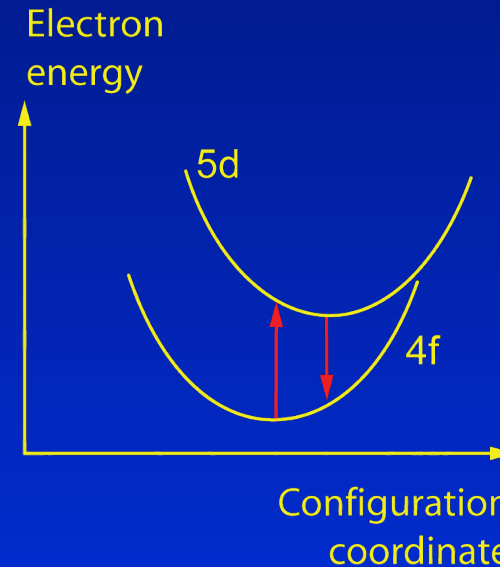
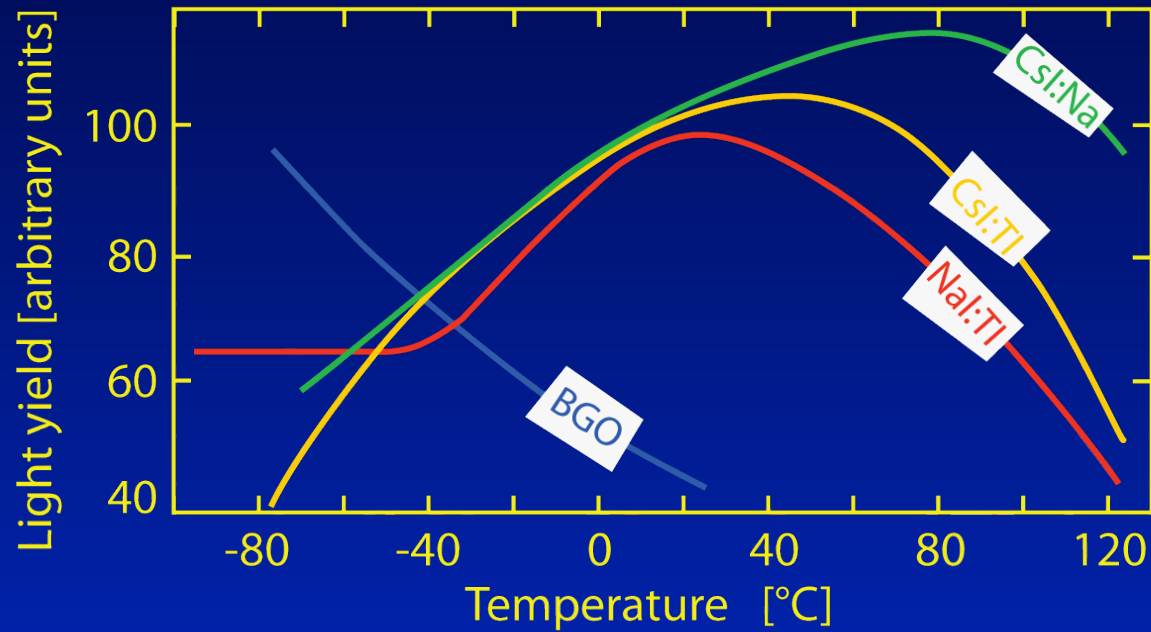
Decay : exponential

BUT ...

- more than one type of luminescence centre
- traps capture electrons and holes
  - > slower rise time
  - > afterglow

# CsI:TI decay spectrum



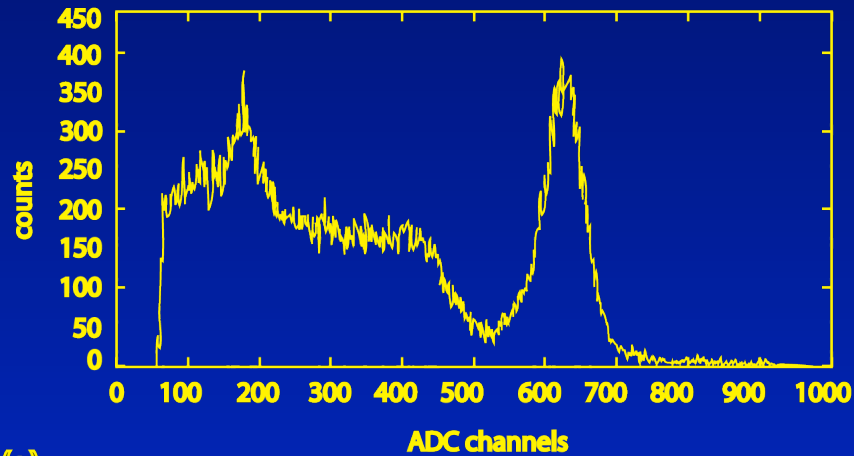


Thermal quenching  
 few scintillators are efficient at elevated  
 temperature

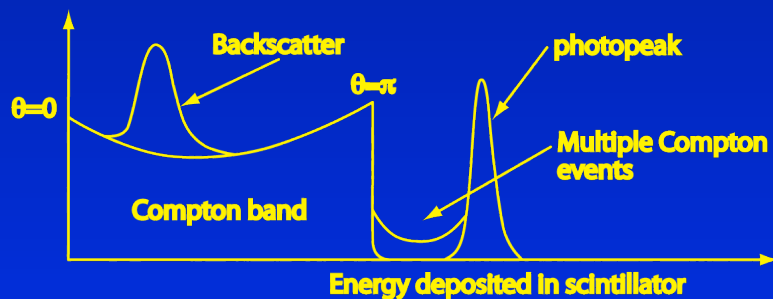
# Applications of inorganic scintillators



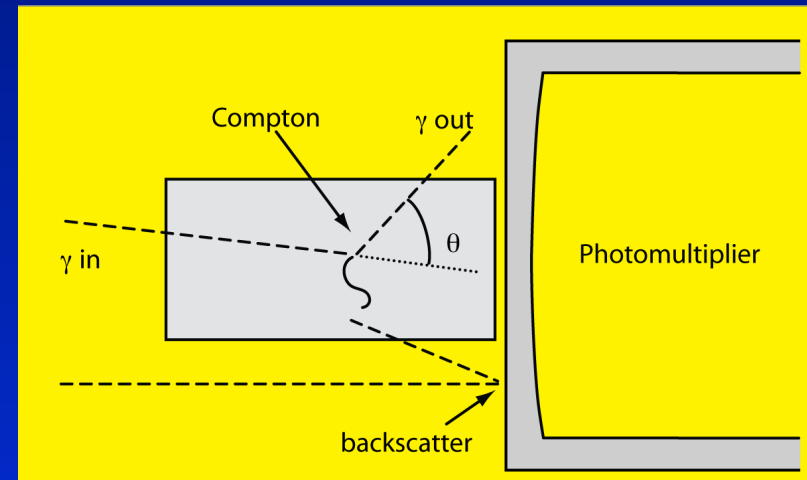
# A keV to MeV gamma ray in a crystal



(a)



(b)



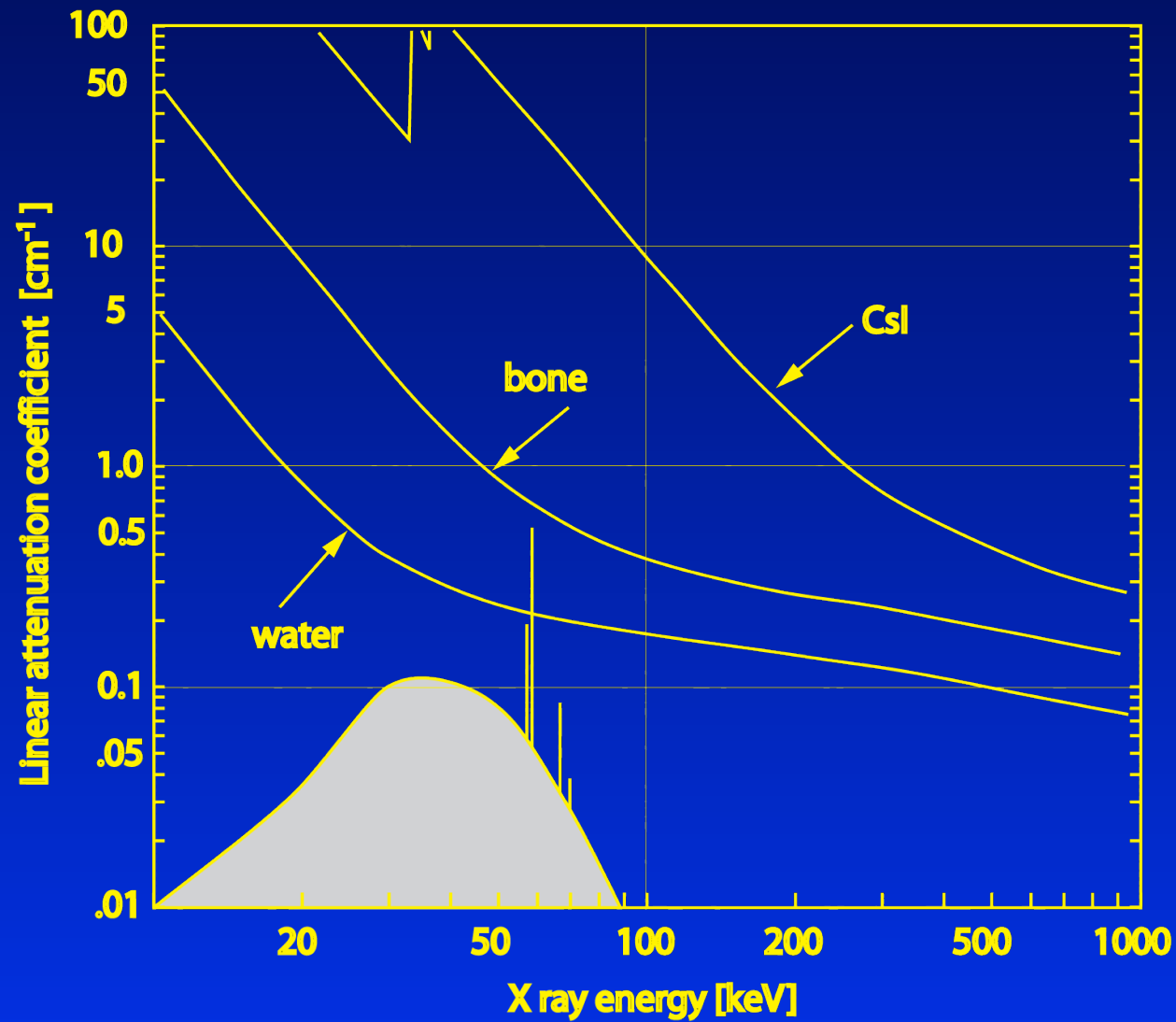
# Scintillators in medicine

X-ray detection, radiology, CT-scanner

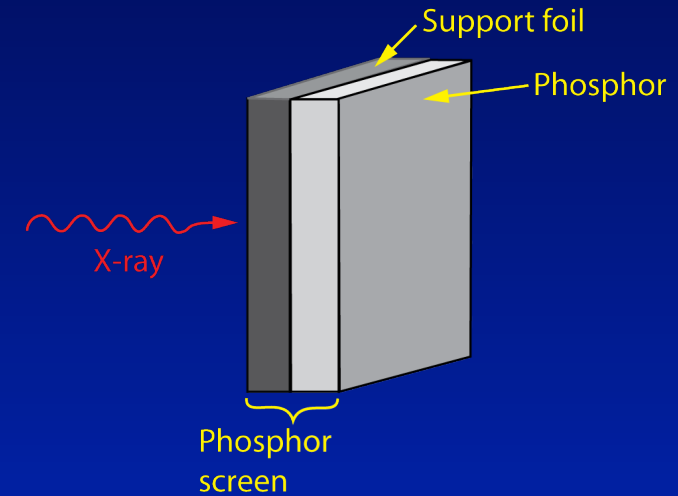
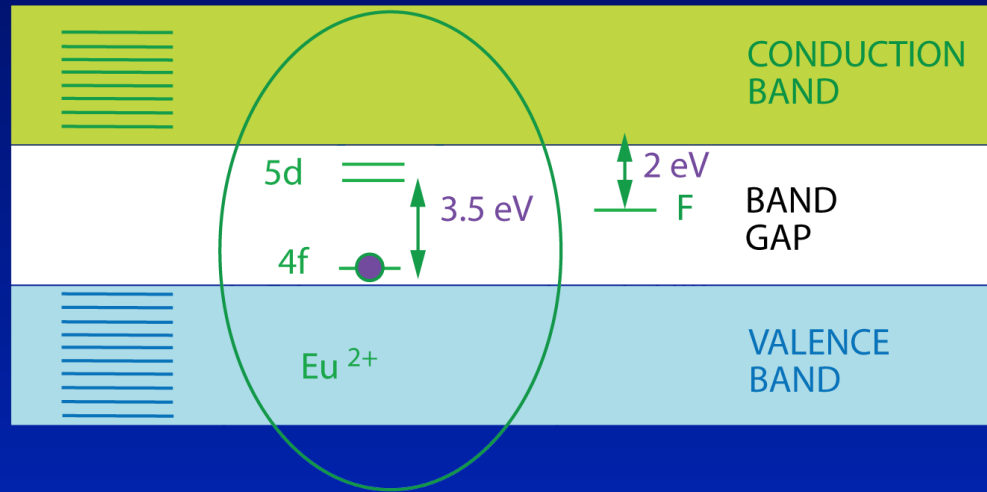
Single gamma detection: scintigraphy,  
SPECT

Positron emission tomography (PET)

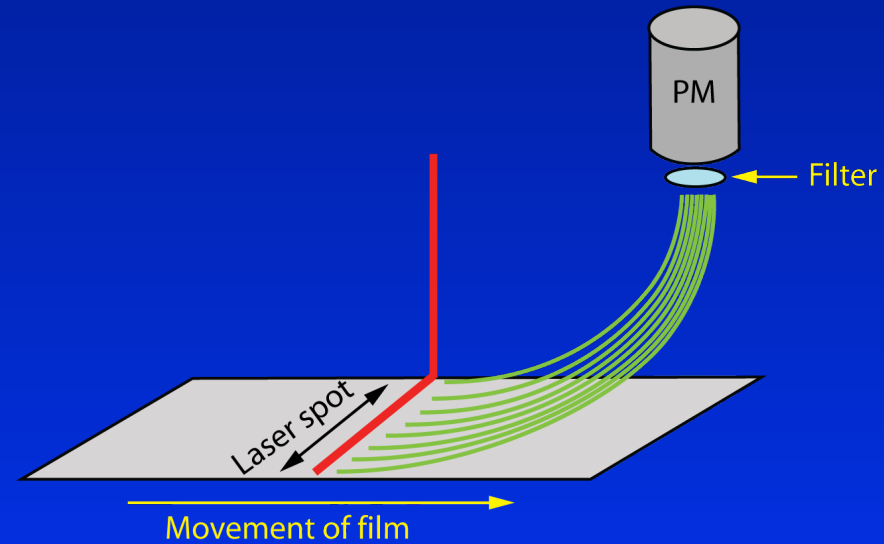
# X-ray detection



# Computed radiography (X-ray imaging)

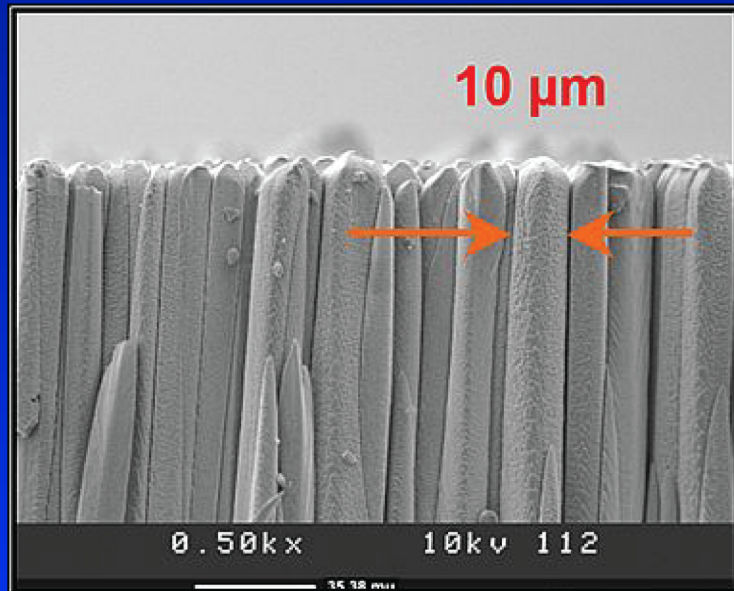
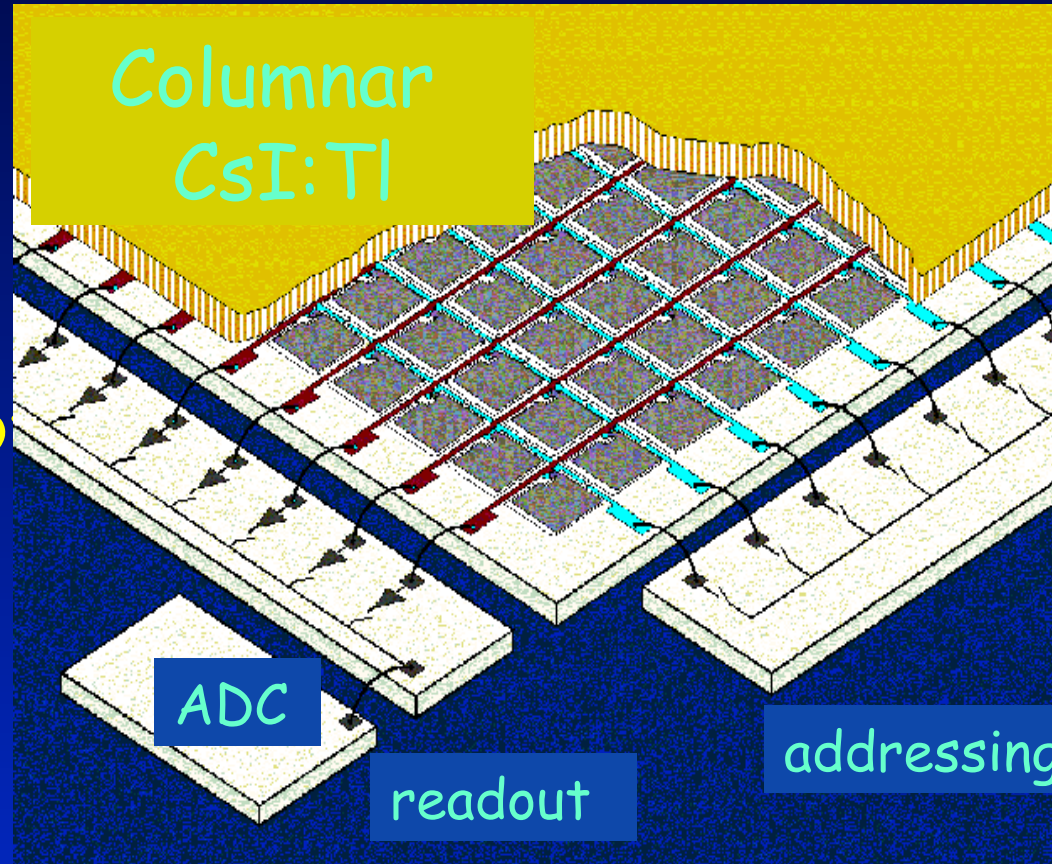


Phosphors  
 $\text{BaFBr:Eu}^{2+}$   
 $\text{BaFI:Eu}^{2+}$ ,  
 $\text{CsBr:Eu}^{2+}$

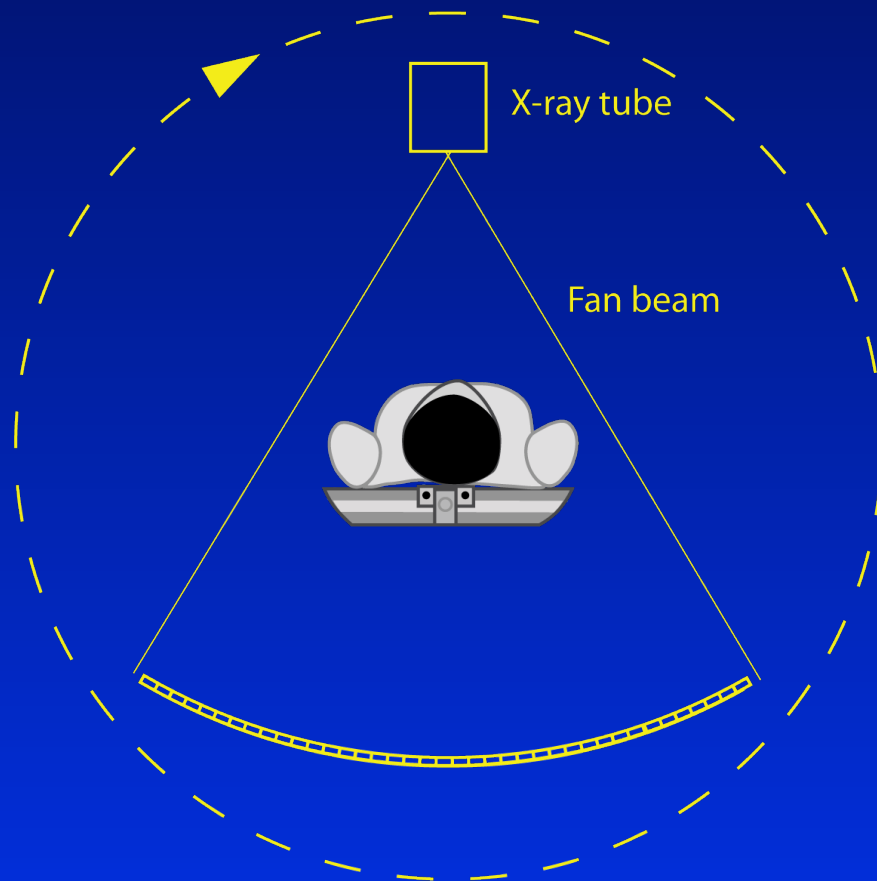


# Digital radiography

Amorphous silicon  
photodiode array  
+CsI:Tl, Eu scintillato



# The CT scanner



A transmission X-ray image is made along to all directions around the patient. Allows reconstruction of the 3D absorption density in the body.

- scintillator + photodiode
- measuring in DC mode

### Commonly use scintillators for CT

	CsI:Tl	CdWO <sub>4</sub>	(Y, Gd) <sub>2</sub> O <sub>3</sub> :Eu <sup>3+</sup>	Gd <sub>2</sub> O <sub>2</sub> S:Pr <sup>3+</sup>
Type	crystal	crystal	ceramic	ceramic
Density	4.52	7.13	5.91	7.34
Emission [nm]	550	580	610	520
Light yield [rel]	100	30	67	75
Decay time [μs]	0.6	8.9	1000	3
Afterglow	yes	no	limited	no

Scintillator requirements: large stopping power, large LY, no afterglow

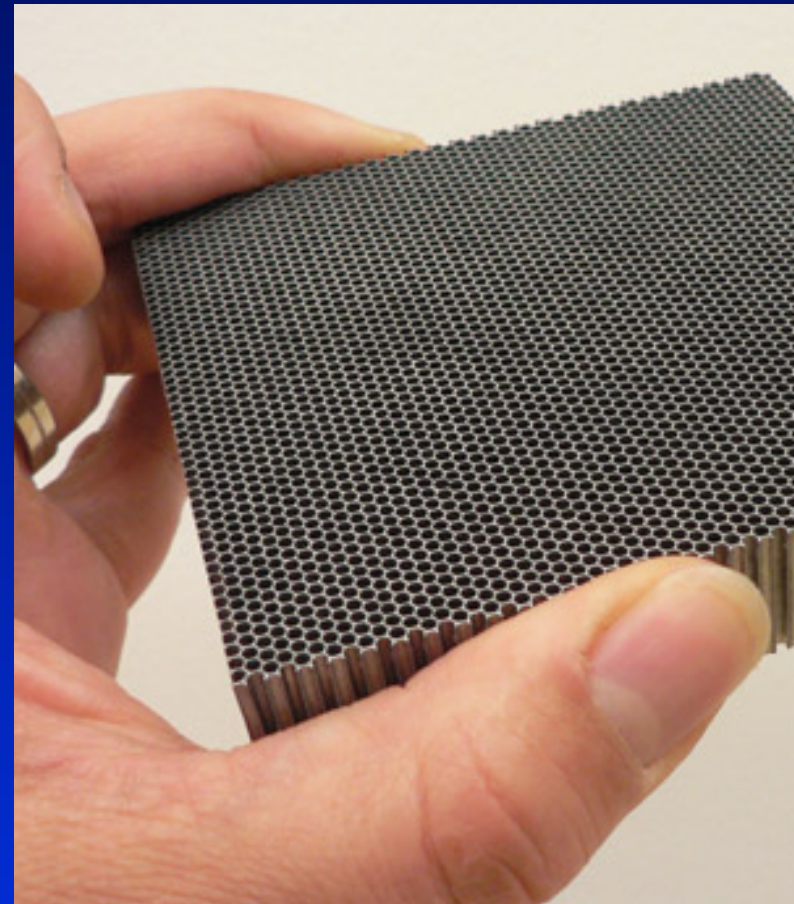
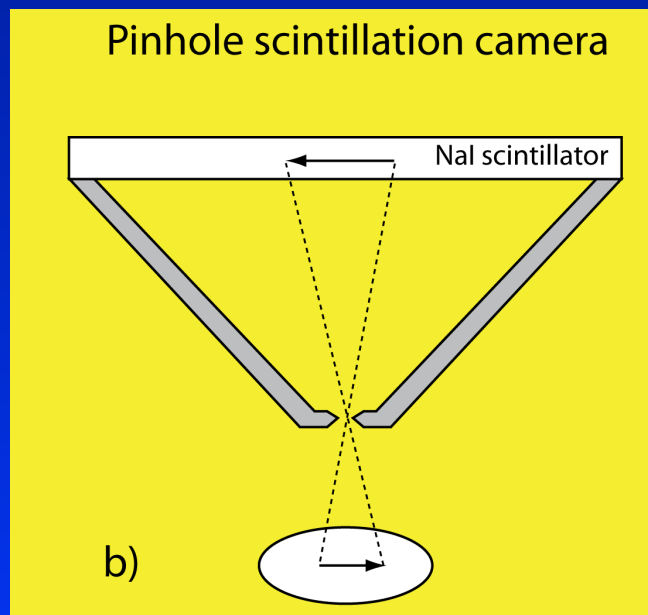
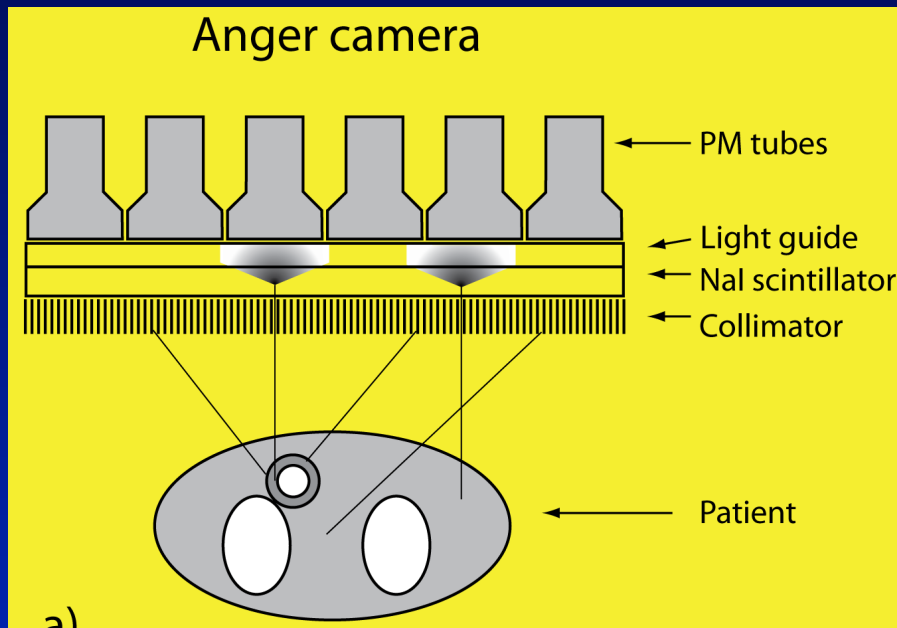
# Nuclear medicine

## Scintigraphy, SPECT & PET

These are non invasive methods for imaging the distribution of a radioactively labelled compounds in the human body. This is often to as "molecular imaging", or functional imaging.



# Scintigraphy: gamma camera (Anger camera)



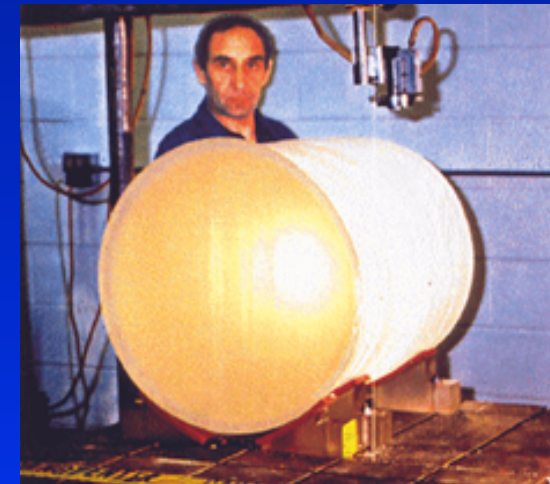
**Table 18.2: Commonly used isotopes in gamma imaging.**

Isotope	Symbol	Half life	Decay	Gamma energies [keV]
technetium-99	$^{99m}\text{Tc}$	6.01 h	IT <sup>(1)</sup>	140(89%)
iodine-123	$^{123}\text{I}$	13.3 h	ec <sup>(2)</sup>	159(83%)
iodine-131	$^{131}\text{I}$	8.02 d	$\beta^-$	364(81%)
thallium-201	$^{201}\text{Tl}$	3.04 d	ec	69-83(94%), 167(10%)
gallium-67	$^{67}\text{Ga}$	3.26 d	ec	93(39%), 185(21%), 300(17%)

(1) IT= isomeric transition, (2) ec=electron capture

Scintillator: NaI;Tl; at 140 keV  
m. f. p.  $\approx$  4 mm.

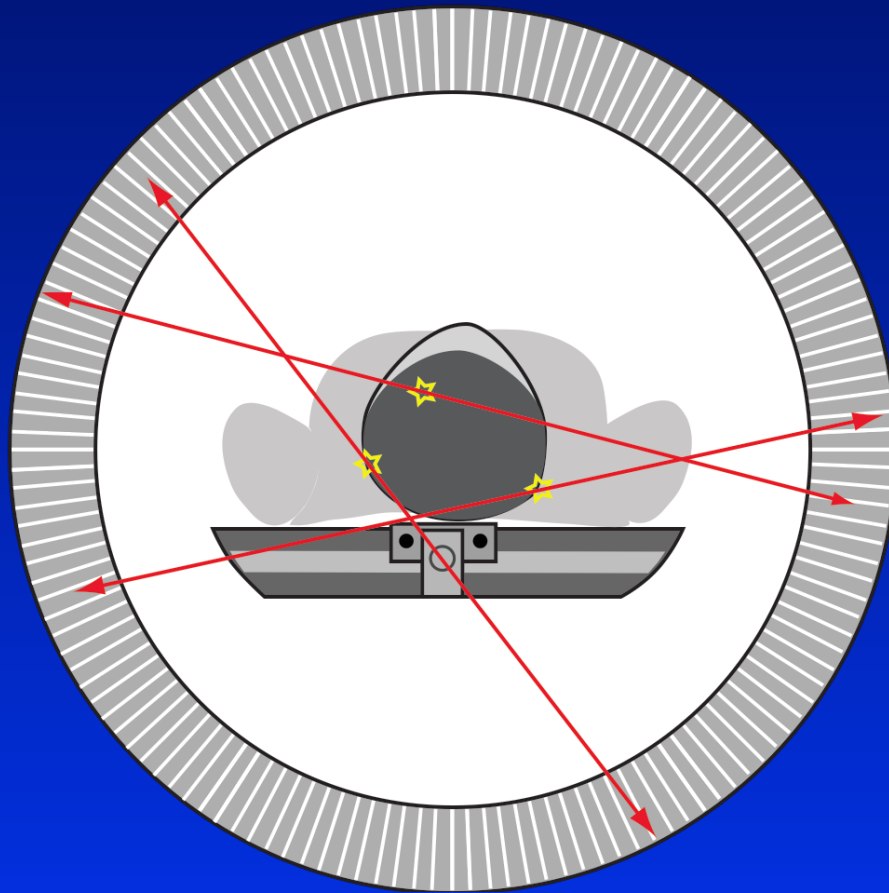
Scintillator requirements: large LY,  
moderately good stopping power,  
moderately good timing



# SPECT: Single Photon Emission Computed Tomography tomographic images with a gamma camera



In Positron Emission Tomography a chemical compound is labelled with a positron emitting isotope. The labelled compound is injected in a patient.



After some time the isotopes decay. The emitted positron annihilates with an electron into two back-to-back gamma rays of 511 keV. Detecting the gamma rays reveals the position of the isotope.

The PET scanner is not observing space points, but a lines of response. The positron annihilation occurred somewhere along this line of response.

From a large set of lines of response, covering a sufficient number of directions around the patient, it is possible to reconstruct the 3-dimensional density distribution of the tracer.

This is usually done with an iterative reconstruction algorithm, and is very computer intensive.





The most commonly used isotopes in PET are

Isotope	Decay time (1/2 life)
---------	-----------------------

$^{11}\text{C}$	20 min
-----------------	--------

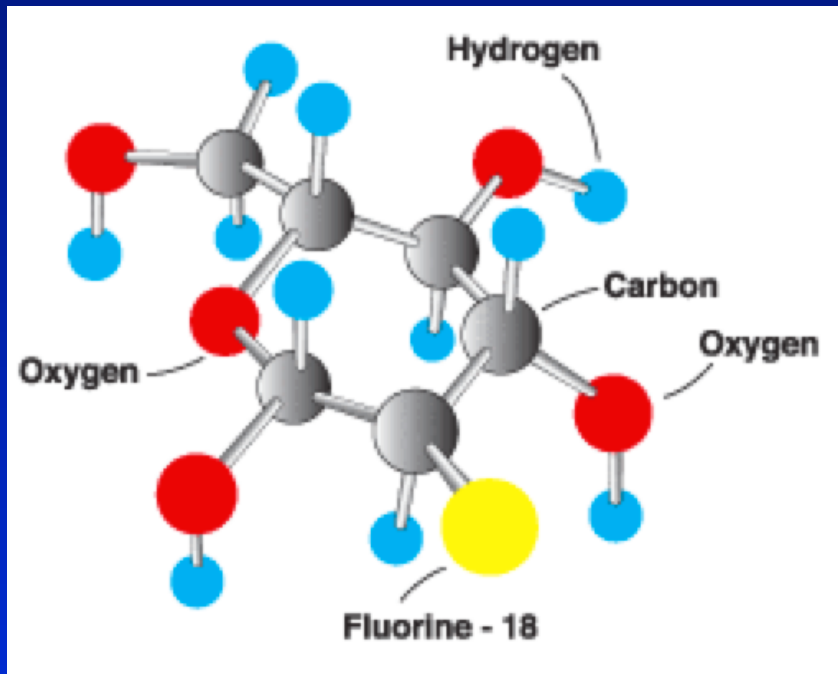
$^{18}\text{F}$	110 min
-----------------	---------

$^{13}\text{N}$	10 min
-----------------	--------

$^{15}\text{O}$	2 min
-----------------	-------

Producing these isotopes requires a cyclotron

By far the most commonly used radiopharmaceutical is FDG (Fluoro2-deoxy-D-glucose), a  $^{18}\text{F}$  labelled glucose analog.



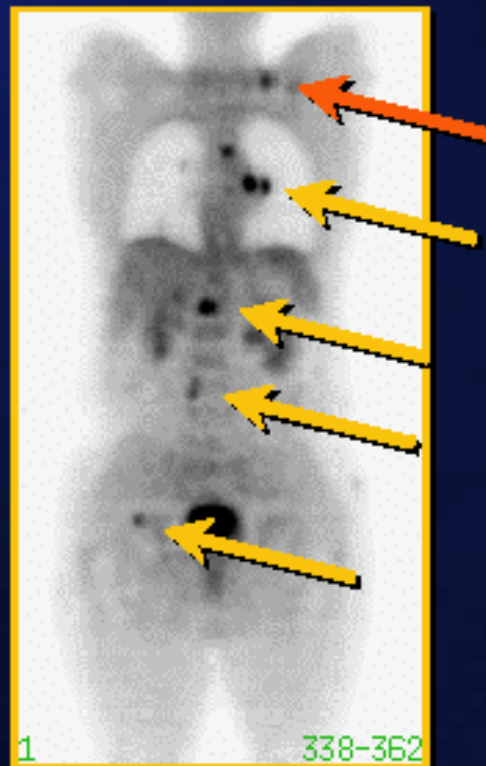
FDG is transported in the body in a very similar way as normal glucose. The metabolic product of FDG is trapped in the cell. Therefore the activity distribution directly reflects the metabolic activity of the cells



# PET Case Study: Melanoma Staging & Follow-up

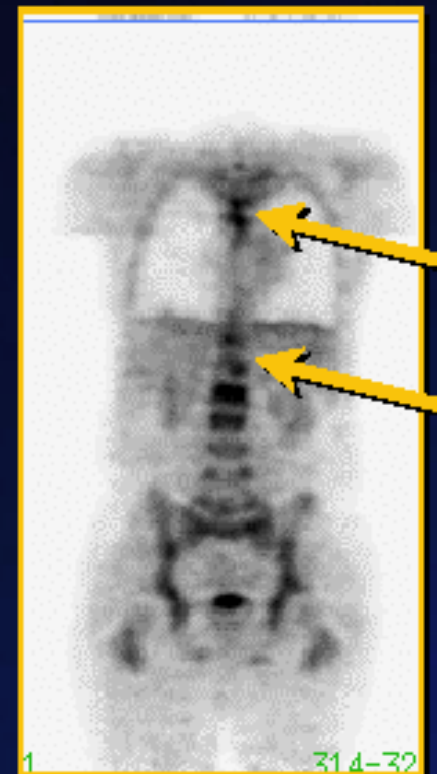
PET in oncology

Before Therapy PET on 11/20/00



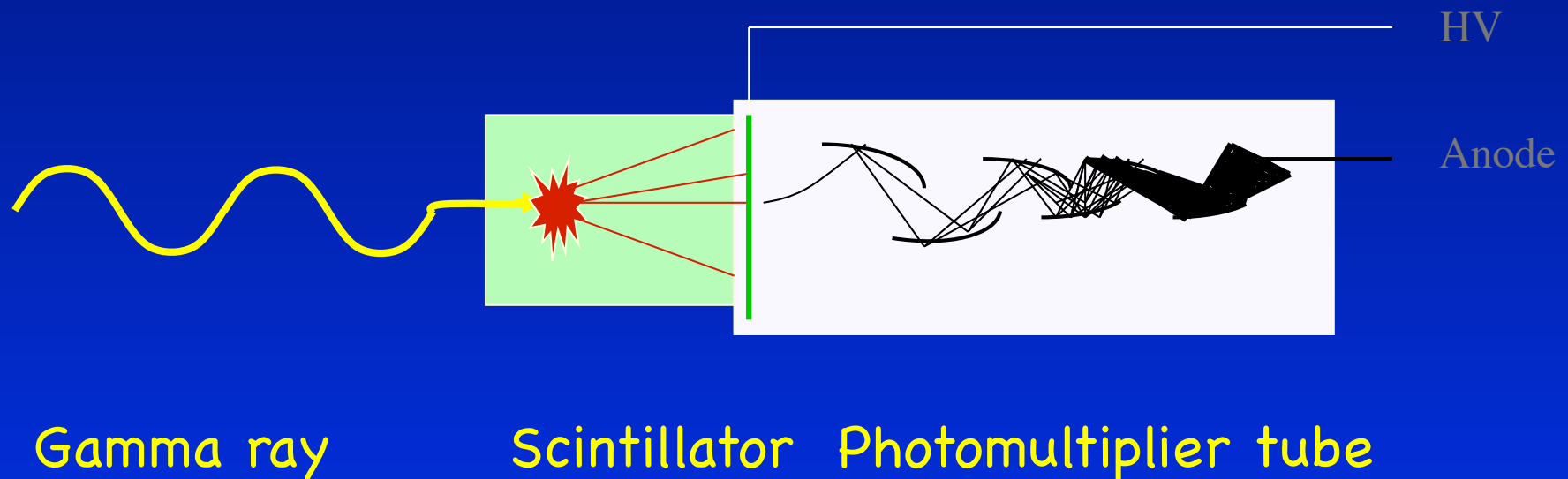
CT showed mass in left shoulder  
But missed abdominal lesions

After Therapy PET on 2/18/01

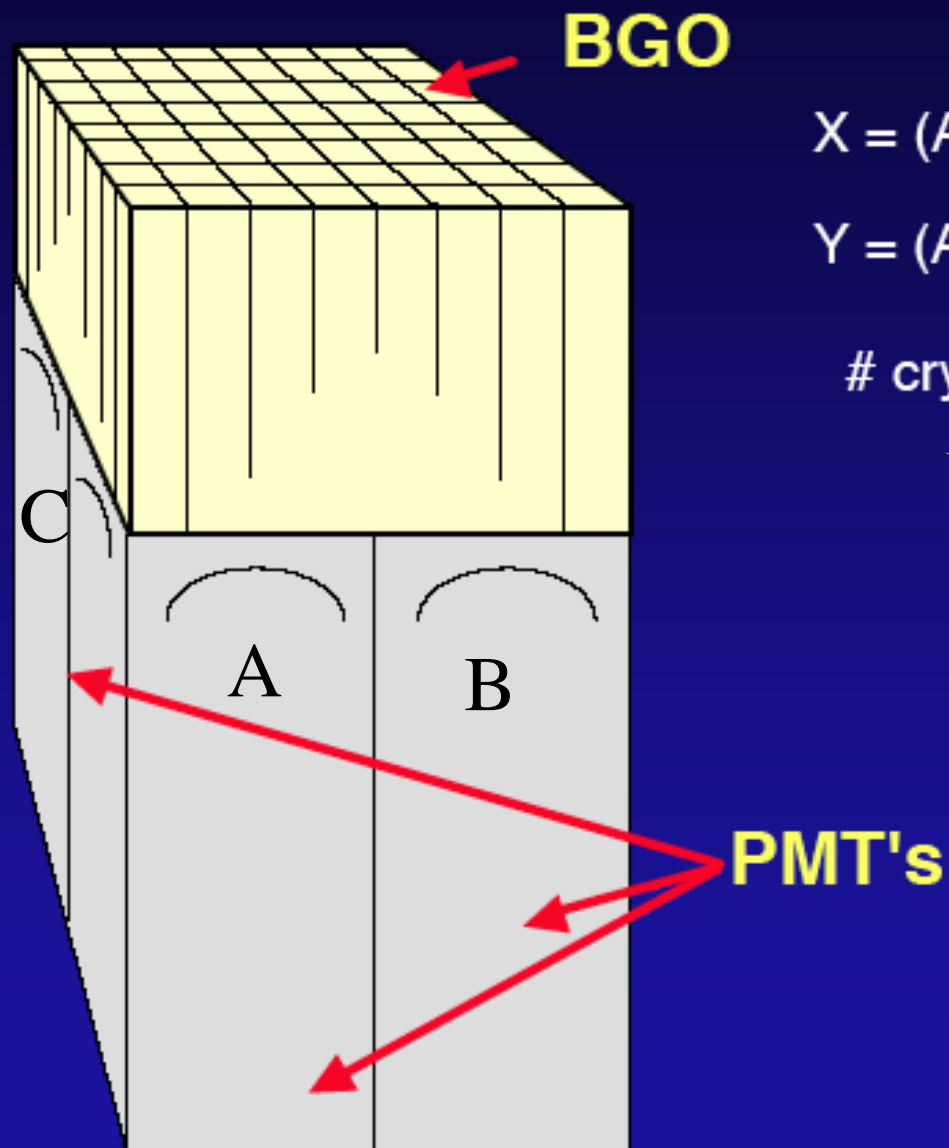


Normal post-therapy  
bone marrow uptake

From the engineering point of view a PET scanner is a detector for 511 keV gamma rays that surrounds the patient.



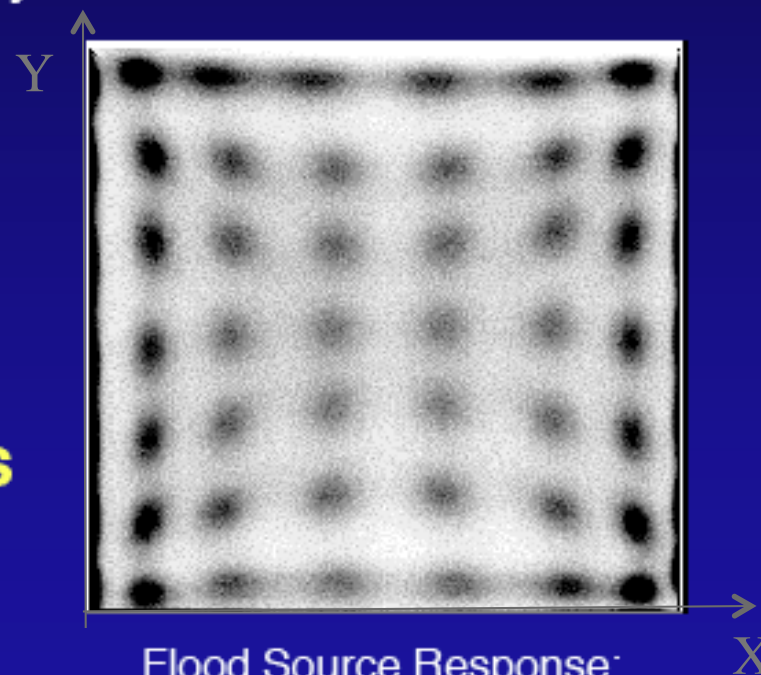
# PET Block Detector



$$X = (A + B - C - D) / (A + B + C + D)$$

$$Y = (A - B + C - D) / (A + B + C + D)$$

# crystals / # PM tubes = 9 to 16



Flood Source Response:  
CTI/Siemens EXACT HR Block

## A PET scanner should have

- spatial resolution in the image
- sensitivity: number of counts/s for a given activity in the patient.
- time resolution
- energy resolution

This needs scintillators with

- fast rise time and decay time
- large light yield
- large stopping power=short absorption length, large photofraction

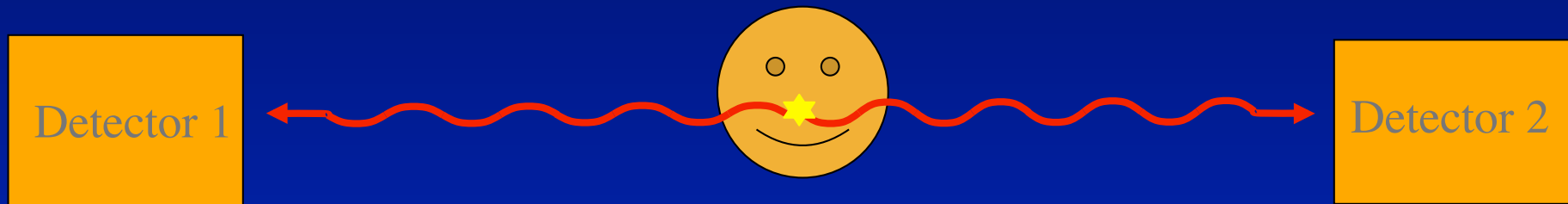
# Scintillators for PET

Crystal	Att. length [mm]@522keV	Light Yield ph./MeV	$\lambda$ [nm]	Decay time [ns]
BGO	10.4	9'000	480	300
NaI	28.6	40'000	410	230
GSO	14.1	8'000	440	60
LSO	11.4	30'000	420	40
LaBr	22.3	70'000	360	35

Time resolution is very important in PET to remove random coincidences

Needs  $\Delta t \approx$  few ns

Time Of Flight (TOF)?  $\Delta x = 15 \text{ cm} \Rightarrow \Delta t = 1 \text{ ns} !$



If  $\Delta t \approx 20 \text{ ps}$  events would be space points !  
Leads to considerable reduction of noise in the image

For best timing, the rise time of the scintillator is very important, LSO has a rise time of 90 ps.  
For materials with negligible rise time

time resolution  $\propto \sqrt{\frac{\tau_{decay}}{N_{pe}}}$

LSO + 0.3% Ca  $\gg$  decay time  $\approx$  30 ns  
LaBr:Ce ? rise time 370/800 ps.

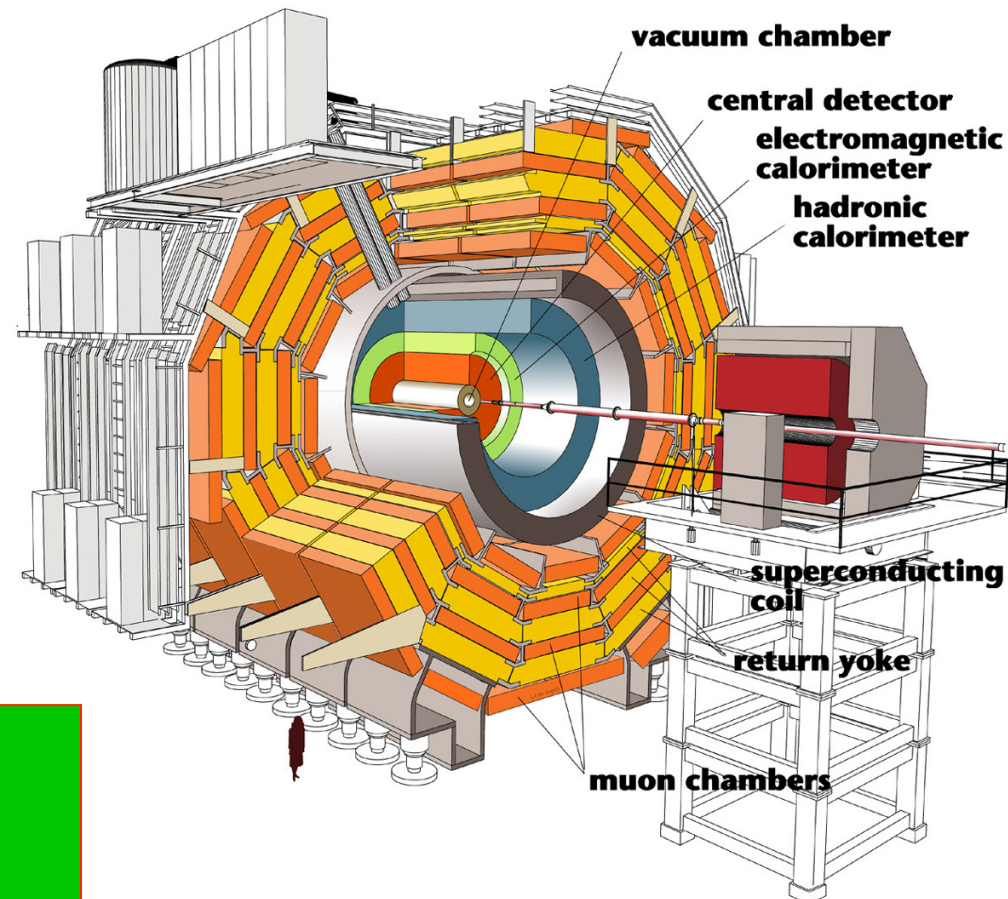


# Scintillators for high energy physics

High energy  $\gg \approx 10$  MeV

Inorganic scintillators provide the best method for the detection of high energy gamma rays, or high energy electrons and positrons

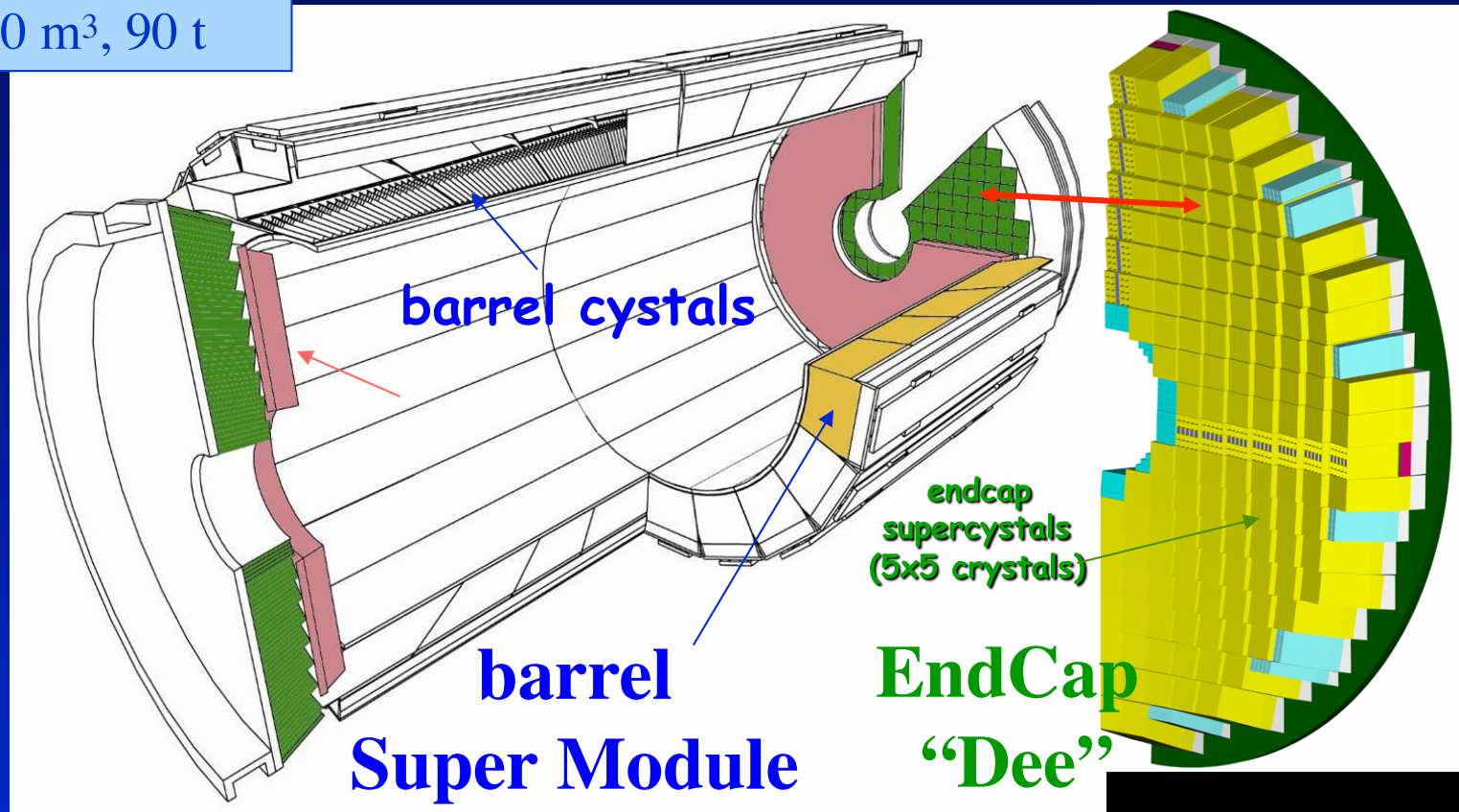
# Compact Muon Solenoid



~ Length ~ 22 m  
~ Diameter ~ 15 m  
~ Weight ~ 14500 t

Needs to detect gamma rays and electrons up to few 100 GeV

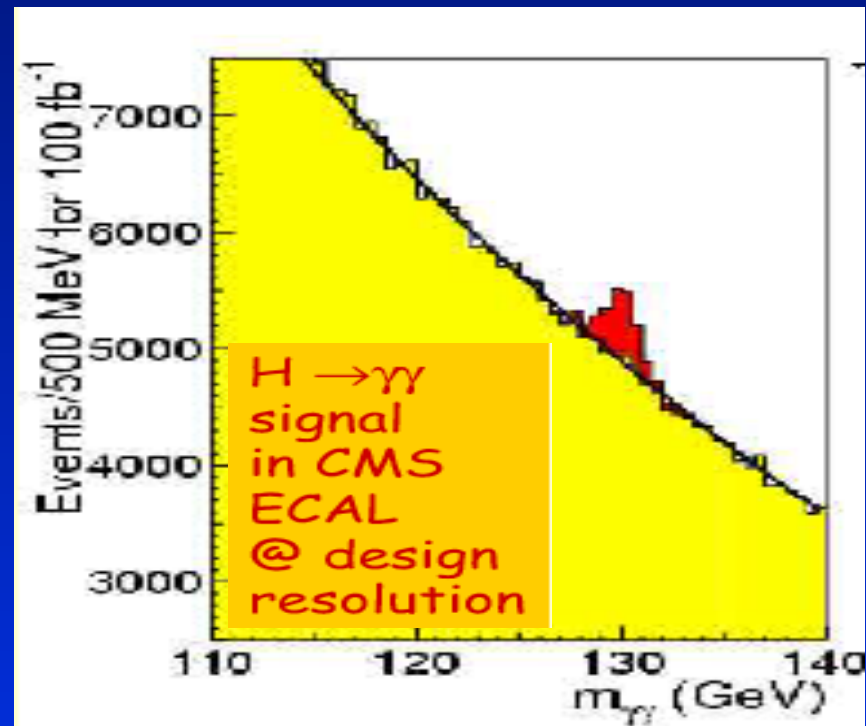
PWO:  $\text{PbWO}_4$   
about 10 m<sup>3</sup>, 90 t



Barrel:  
36 Super Modules  
61200 crystals (2x2x23cm<sup>3</sup>)

EndCaps:  
4 Dees  
14648 crystals (3x3x22cm<sup>3</sup>)

For a light B\_E\_Higgs (only possibility left )  $H \rightarrow \gamma\gamma$  best channel. Narrow width, irreducible background:  
ECAL resolution is crucial !



The main property of a calorimeter is its energy resolution

$$\frac{\sigma\{E\}}{E} = \sqrt{\frac{a^2}{E[\text{GeV}]} + b^2}$$

$$a=0.02-0.03; b=0.005-0.01$$

- statistical term: depends on light yield but also many other things, e.g, shower is not fully contained
- Constant term: mainly an issue of calibration

# Scintillator requirements for high energy physics

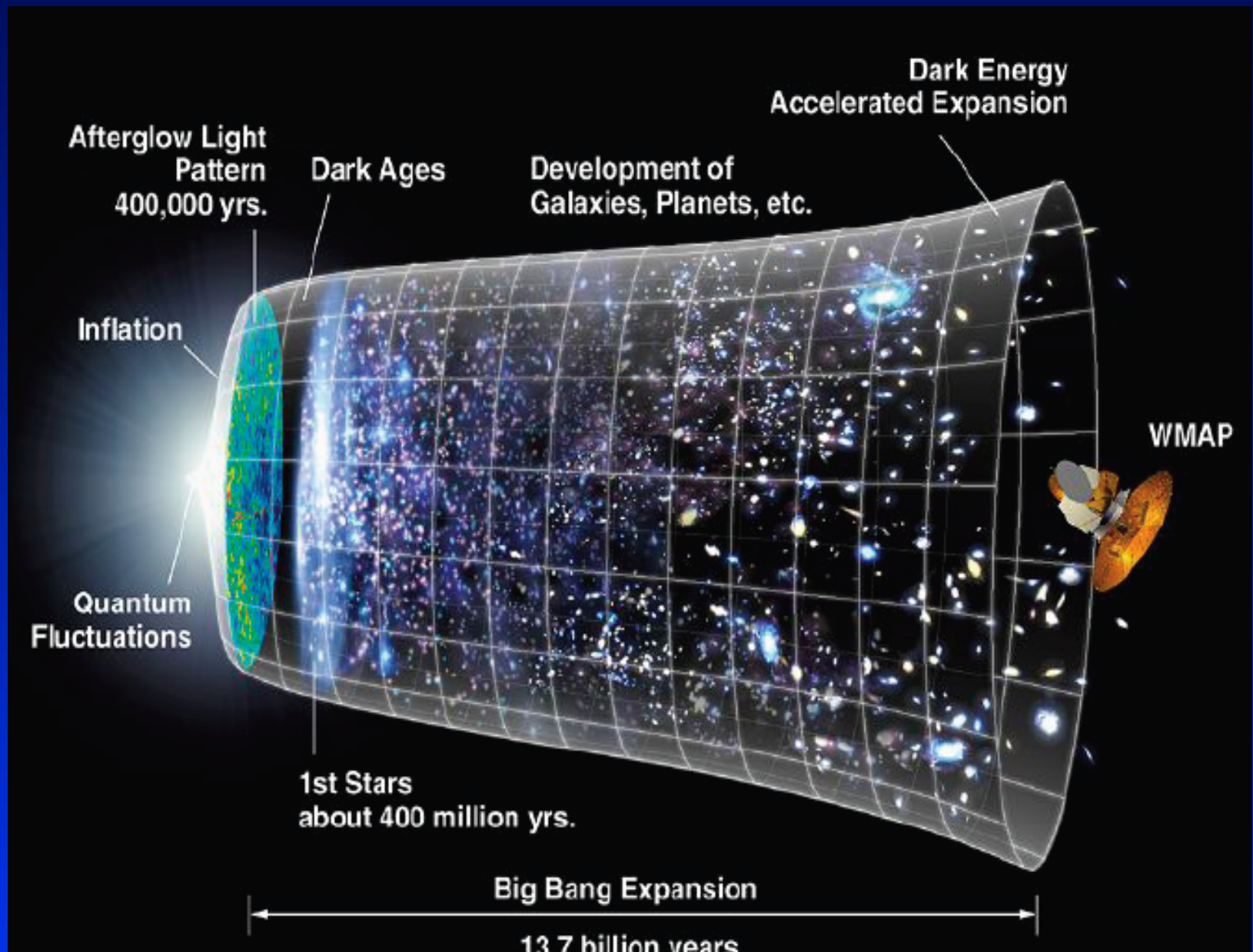
- **stopping power**, short radiation length  $X_0$
- Molière radius  $R_m = 0.035 \times X_0 \times (Z + 1.4)$
- decay time
- **radiation hardness**
- light yield far less important if mainly very high energy gamma rays need to be detected

# Some popular crystals in HEP

	NaI(Tl)	BaF <sub>2</sub>	CsI(Tl)	CeF <sub>3</sub>	BGO Bi <sub>4</sub> Ge <sub>3</sub> O <sub>12</sub>	PWO PbWO <sub>4</sub>
X <sub>o</sub> [cm]	2.59	2.03	1.86	1.66	1.12	0.92 😊
ρ [g/cm <sup>3</sup> ]	3.67	4.89	4.53	6.16	7.13	8.2
τ [ns]	230	0.6 620	1050	30	340	15 😊
λ [nm]	415	230 310	550	310 340	480	420
n@λ <sub>max</sub>	1.85	1.56	1.80	1.68	2.15	2.3
LY [%NaI]	100 😊	5 16	85 😊	5	10	0.5 😞

# Scintillators in astronomy and dark matter searches





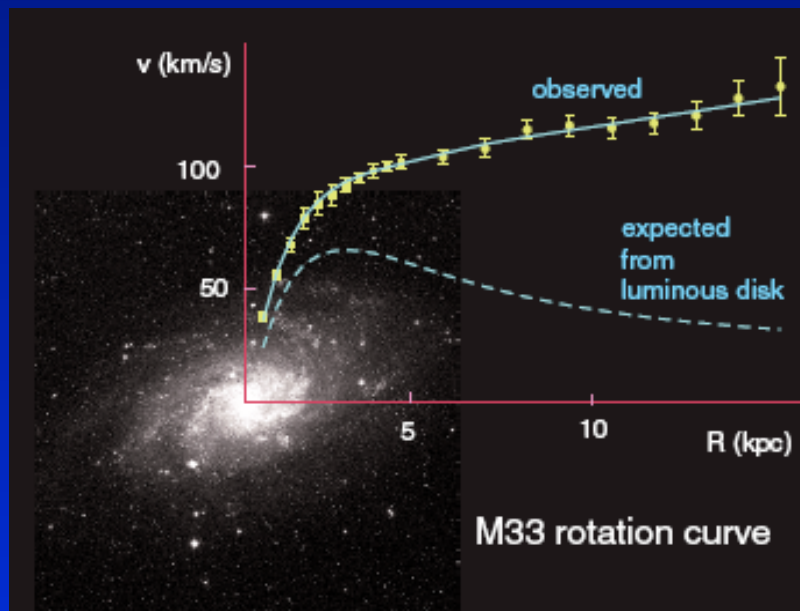
# WIMP-Dark matter searches

## Evidence of Dark Matter Rotation curve of spiral galaxies

Direct detection – elastic scattering off nuclei

### Features:

1. Low energy recoil  $\rightarrow$  ( $\approx 20$  keV)  
 $E = 1/2 M v^2$ .  $(v/c)^2 \sim A$
2. Expected event rate  $\approx 1/\text{kg year}$   
 $\sigma \sim A^2$



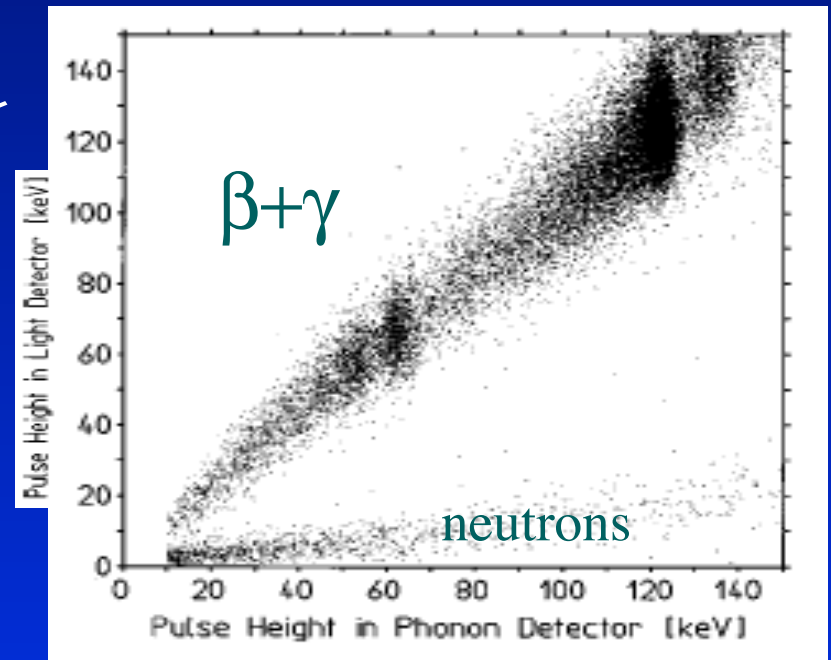
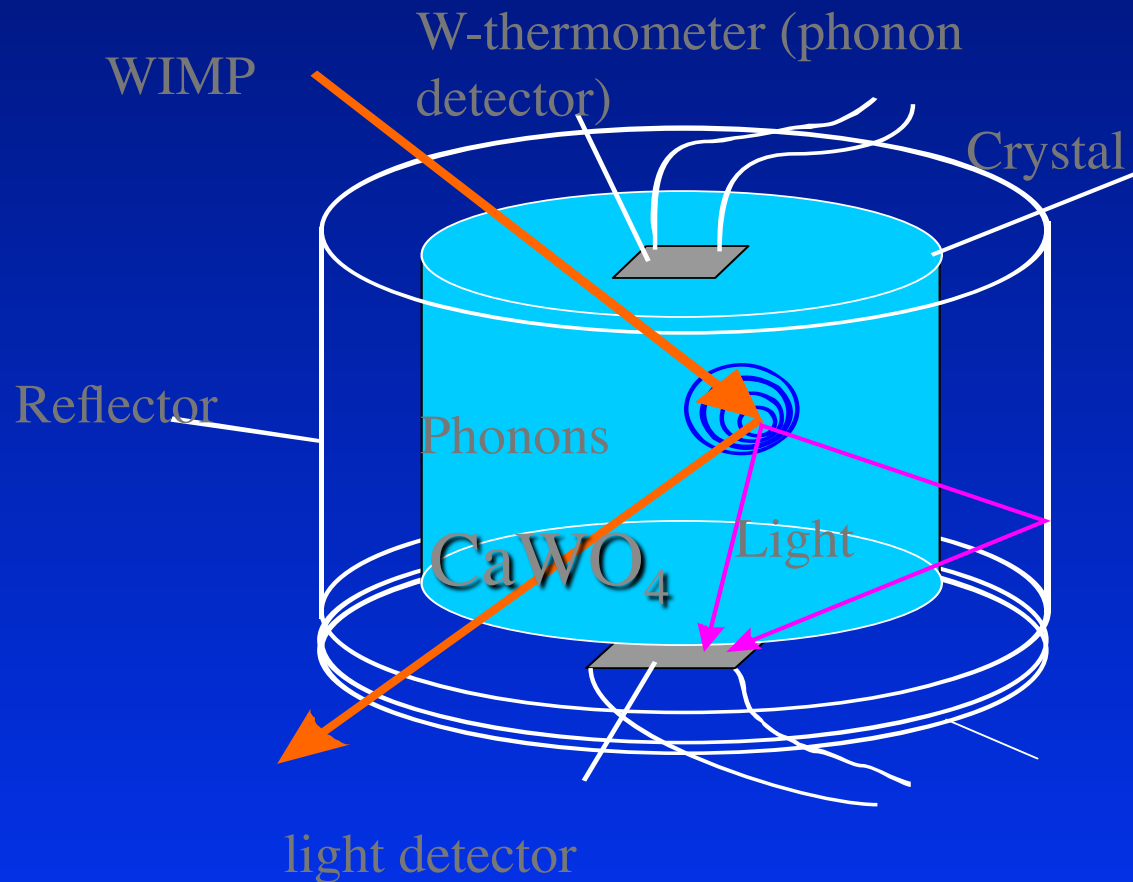
L.Bergstrom Rep.Progr.Phys.63 (2000) 793

$$V = (GM/r)^{1/2}$$

- Background rejection
- Detector mass  $\approx 1000$  kg

# CRESST detector

- Gamma rejection using simultaneous observation of the light signal and heat signal.



P.Meunier et al, Appl.Phys.Let 75 (1999) 1335

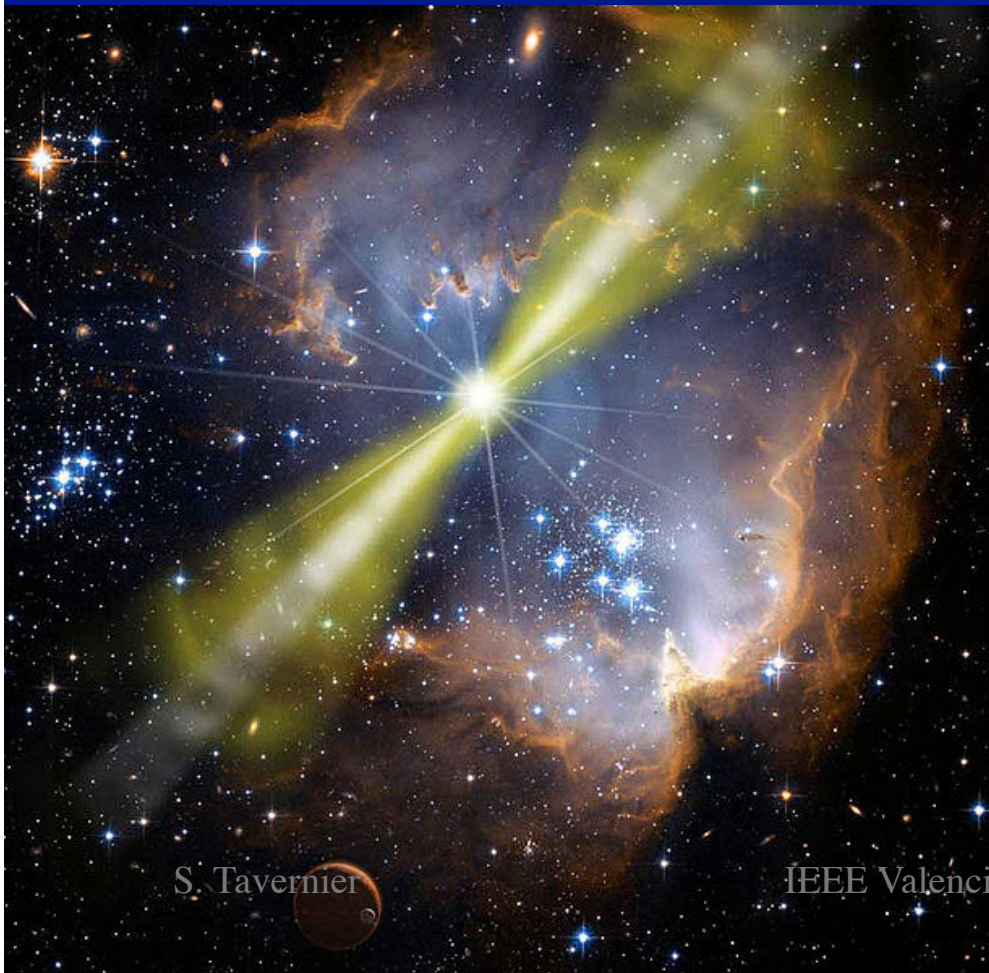
# Scintillator requirements

- high light yield at low temperatures
  - ✓ large atomic number  $A$
  - ✓ large light yield
- Radiopurity (ex Lu, Rb, K, U, Th)
- Suitable thermodynamics characteristics
- Possible candidates
  - ✓  $\text{CaWO}_4$  – satisfactory choice, currently in use, large ongoing effort to improve the material
  - ✓  $\text{ZnWO}_4$  – scintillator under development for cryogenic application
  - ✓  $\text{CaMoO}_4$  and  $\text{CdMoO}_4$  – material under investigation



# Gamma ray astronomy

Gamma rays are absorbed by the atmosphere and must be studied a satellite or balloon born observatory

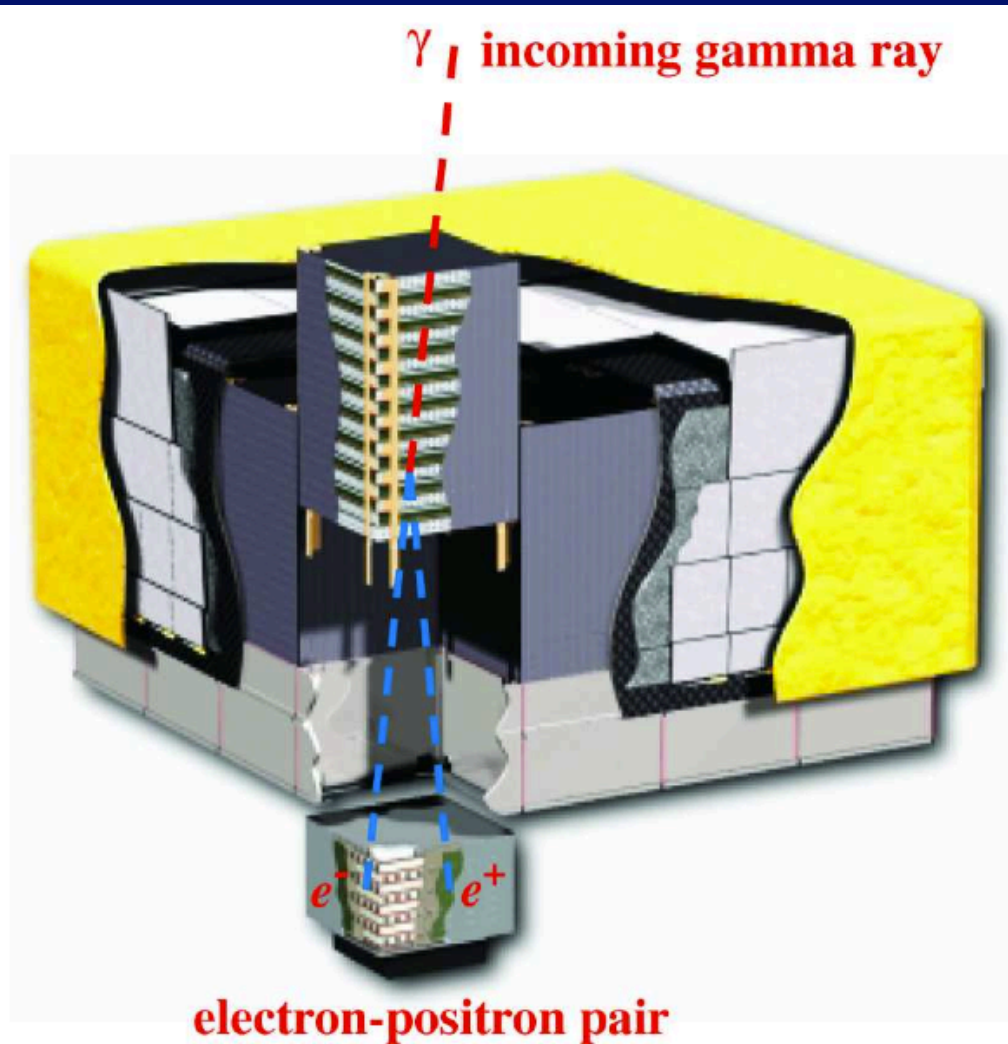


Gamma ray bursts (GRB)  
- are short energetic gamma bursts from distant galaxies  
- allow us to see a glimpse of the most violent events universe

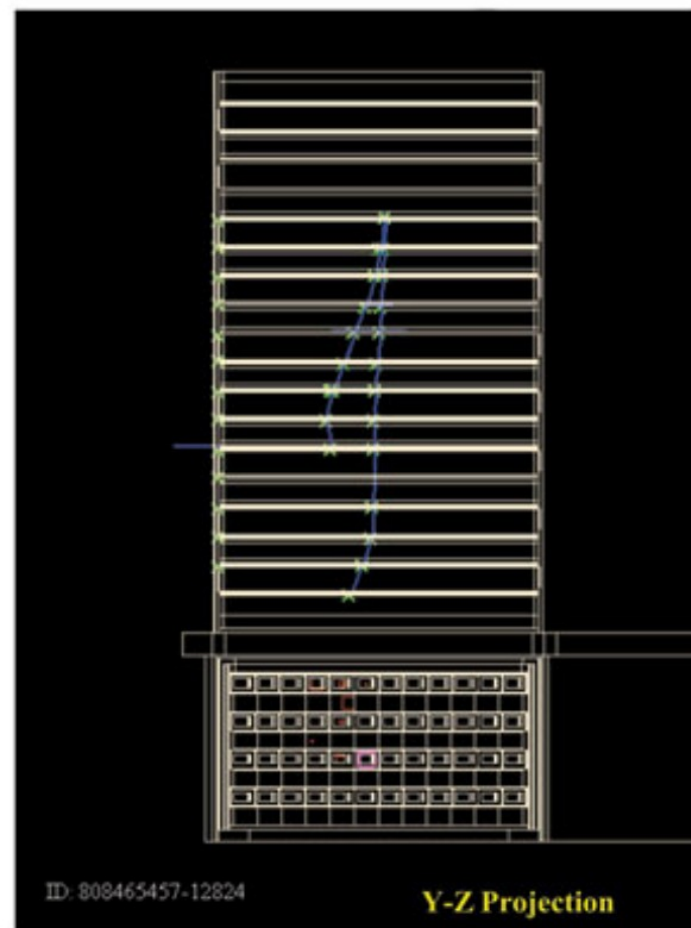
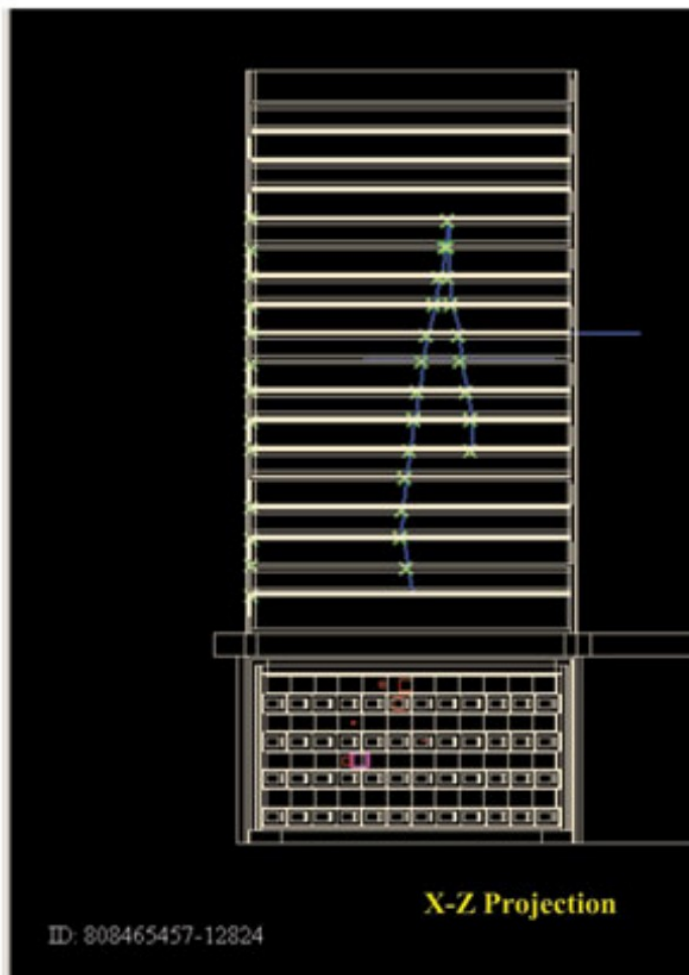
# Fermi Gamma Ray Space Telescope FGST- launched 2008

## Large Area Telescope

- tungsten sheets
- silicon microstrip chambers
- CsI Scintillator with photodiode readout



# Fermi GST- LAT, candidate gamma event



Candidate Gamma-ray Event in 1<sup>st</sup> LAT Flight Tower

## Scintillators have many other applications

- Oil drilling
- Security
- Planetary exploration



# Conclusion & Outlook

- This overview of instrumentation for the detection of subatomic particle is obviously incomplete. Not discussed: superconducting detectors, liquid ionisation detectors, large water or ice Cherenkov detectors etc.
- The field of particle detection is rapidly evolving, but detectors based on ionisation in gases, on ionisation in semiconductors and on scintillation are probably here to stay.
- The importance and role of electronics and software will continue to increase. Progress in micromachining and nanotechnologies will allow making types of detectors we have no idea of today.